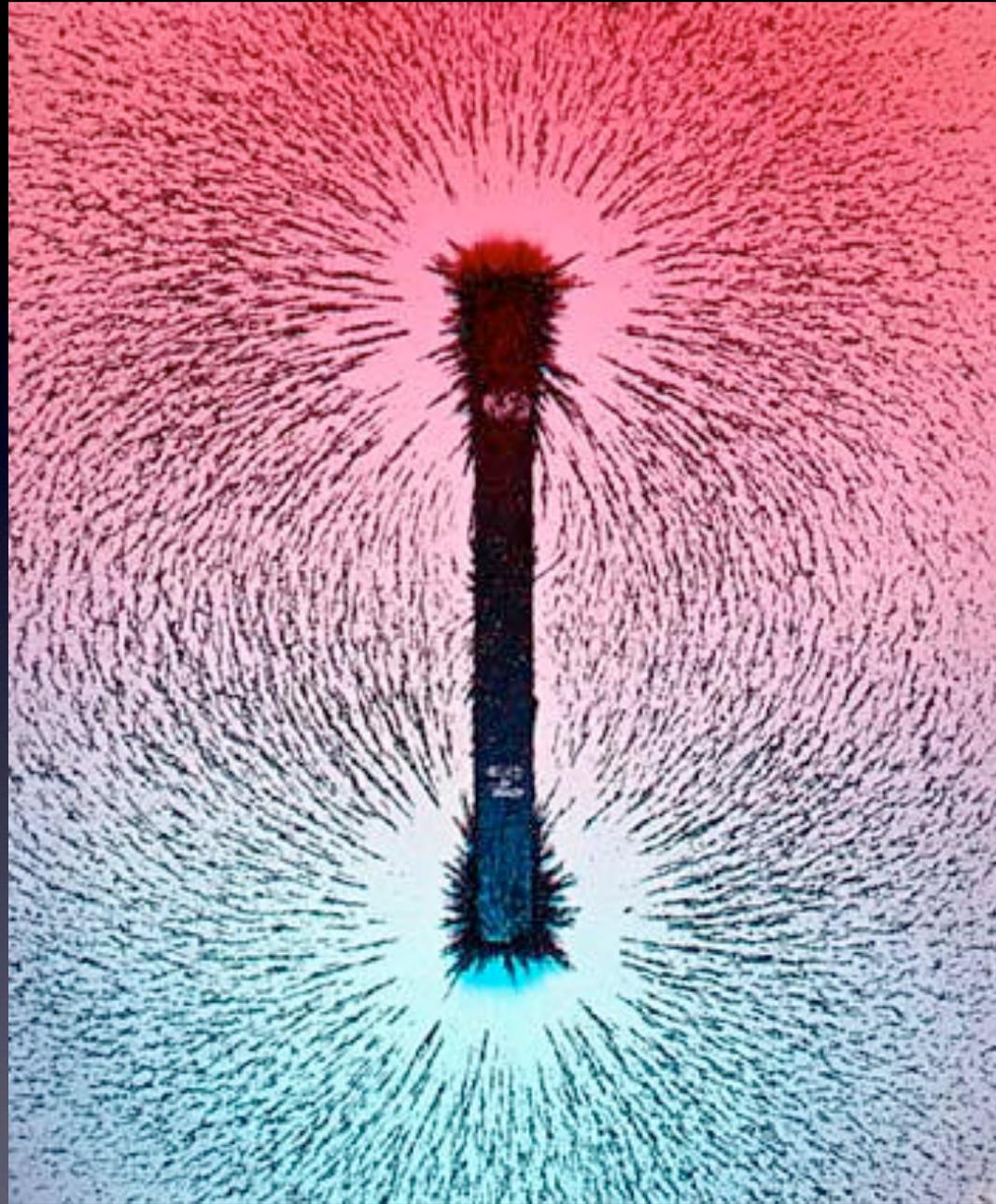


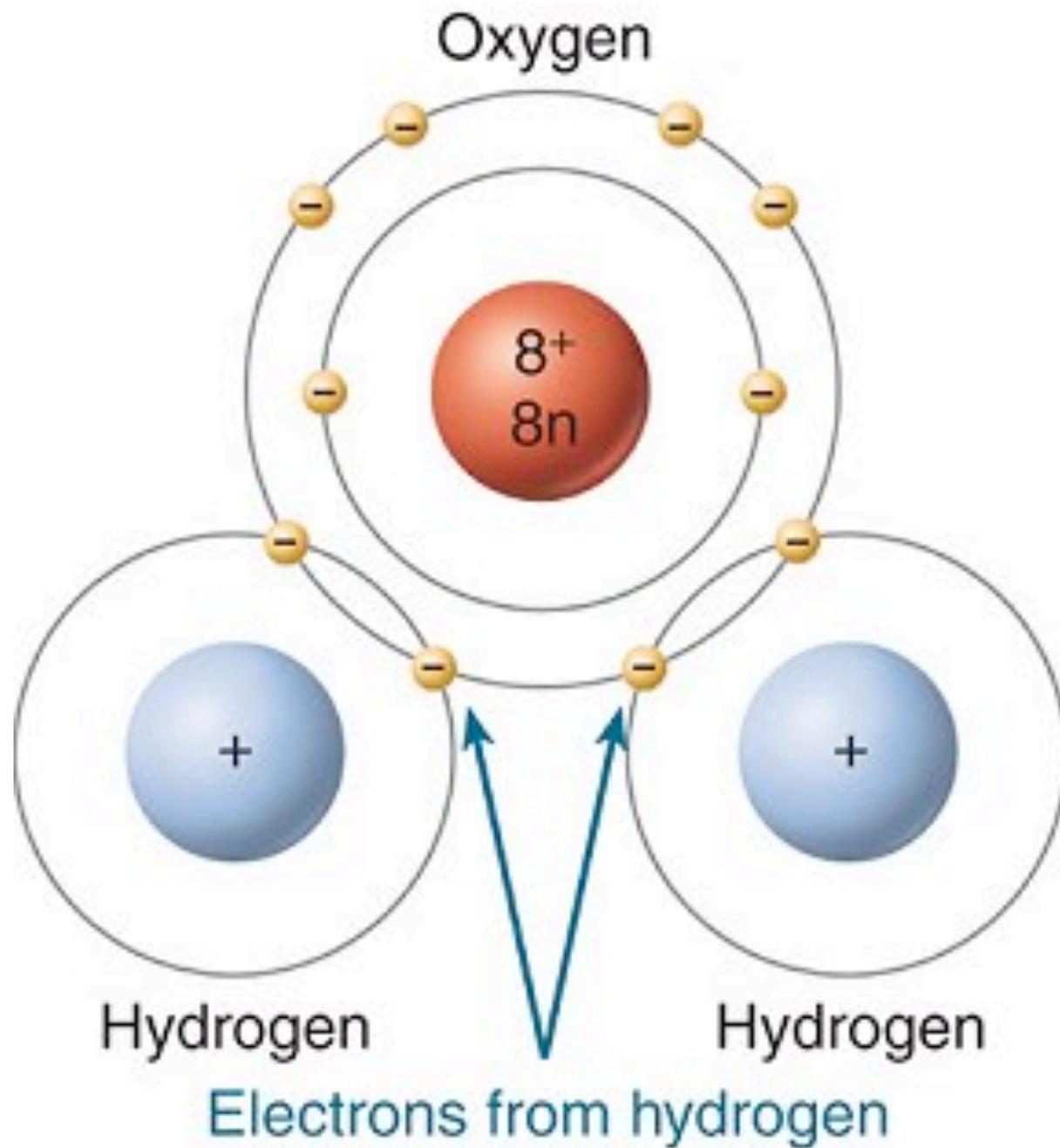
A Non-Physicist's Intro to MRI

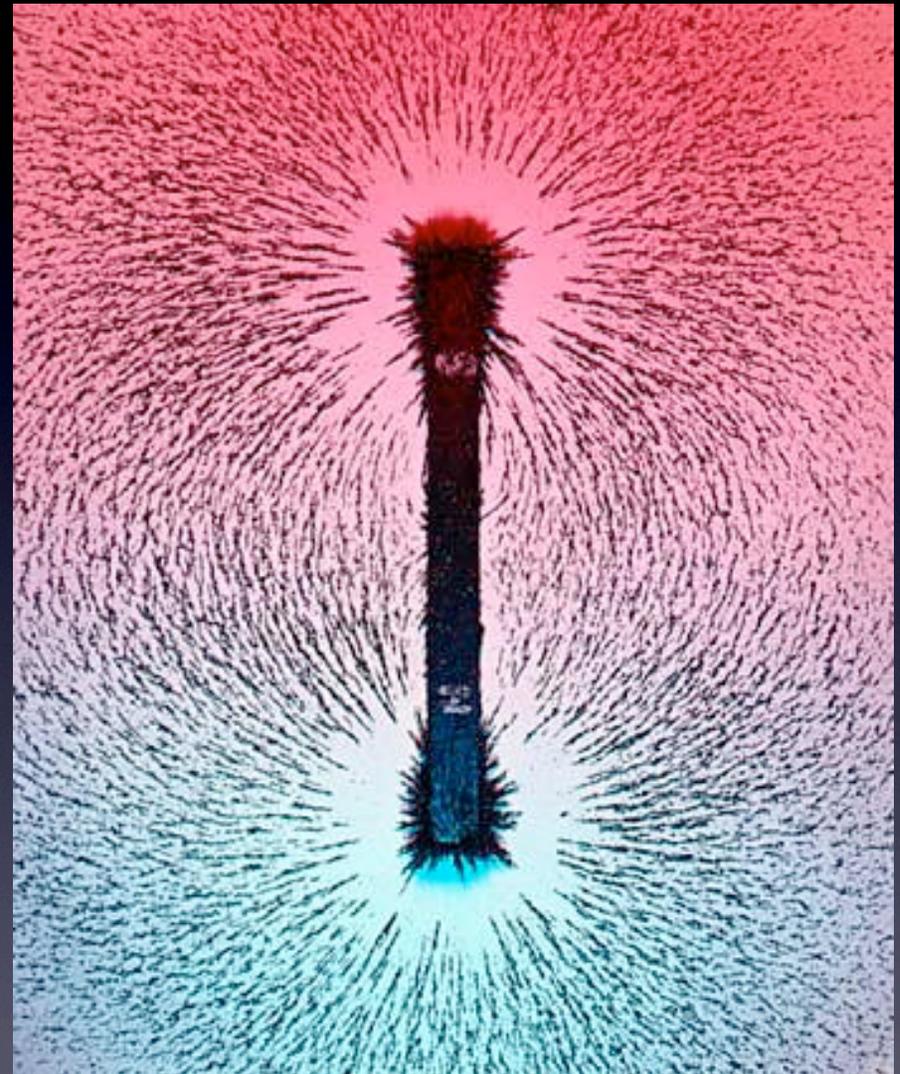
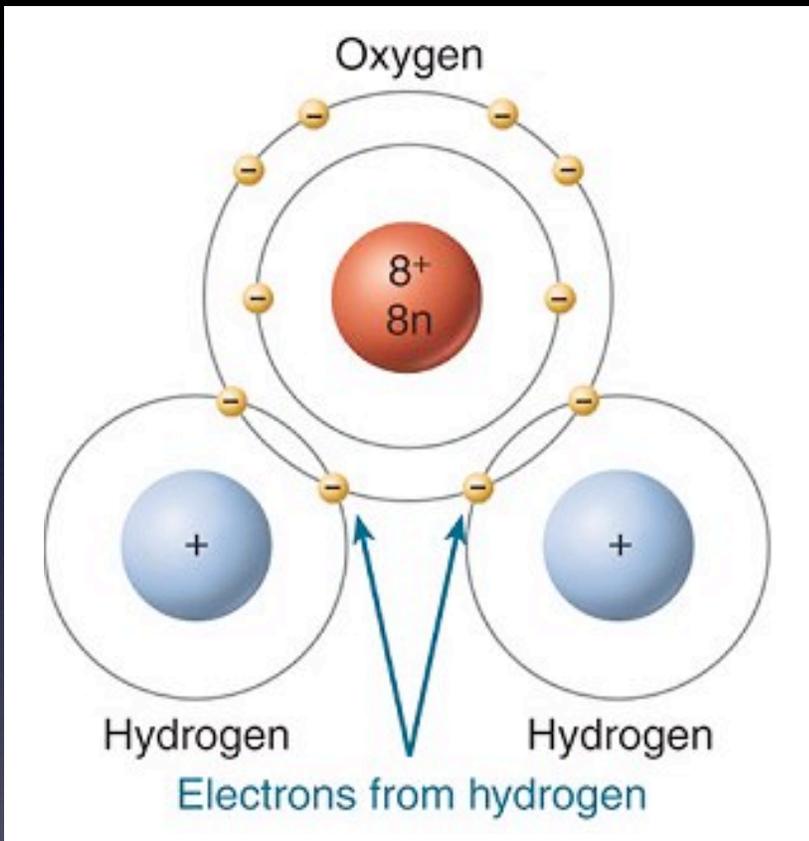
Dylan Tisdall
April 2013



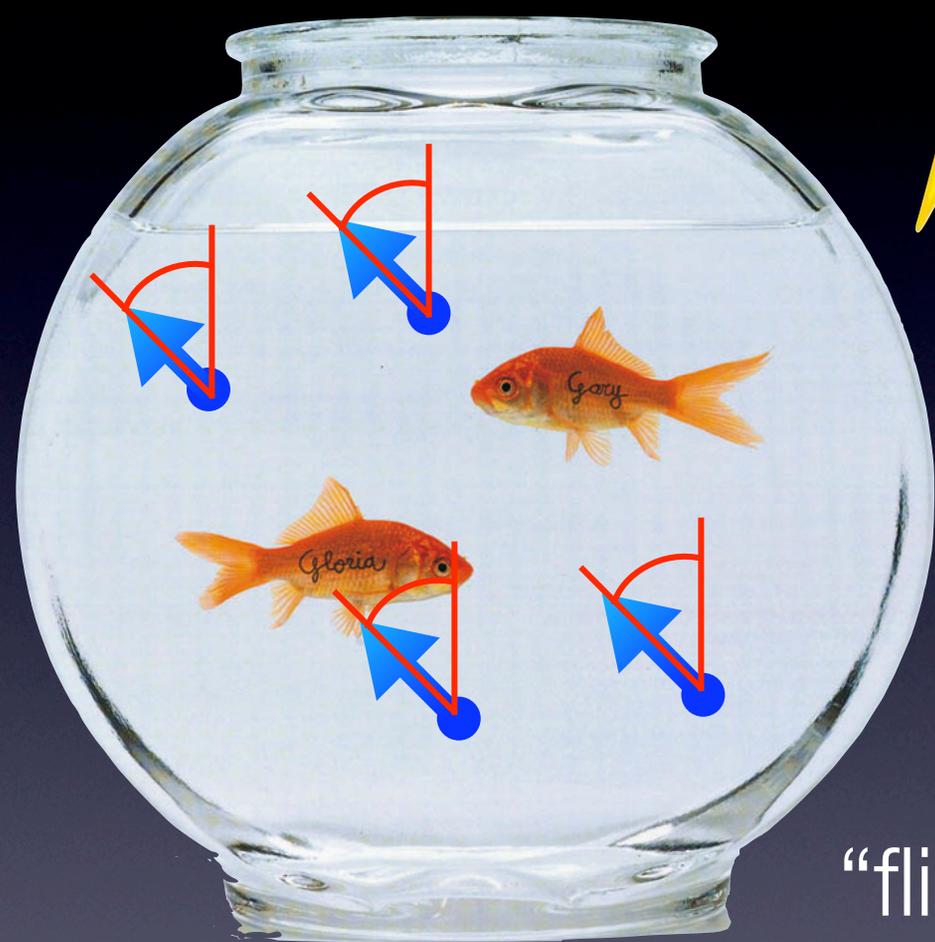


A human head



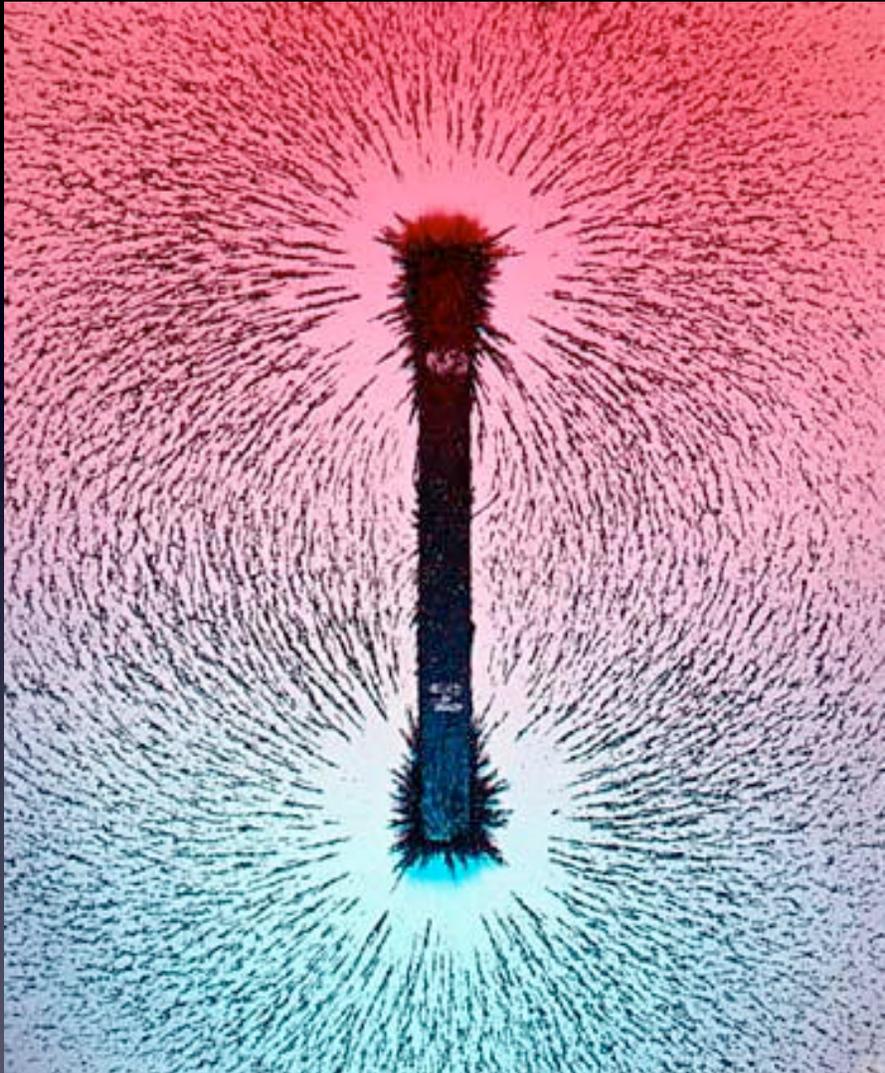


main
magnetic
field

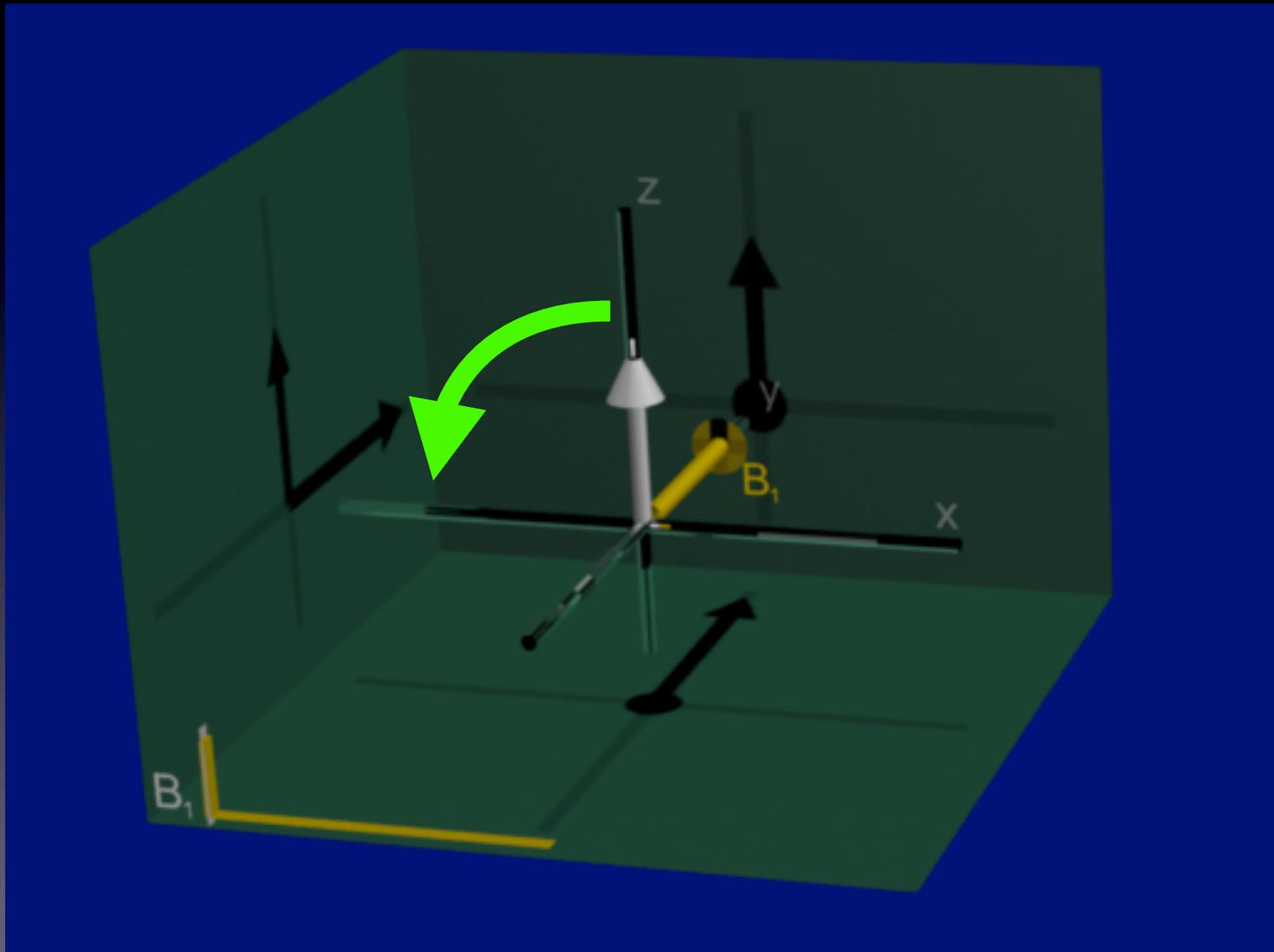


“pulse”

“flip angle”



precession

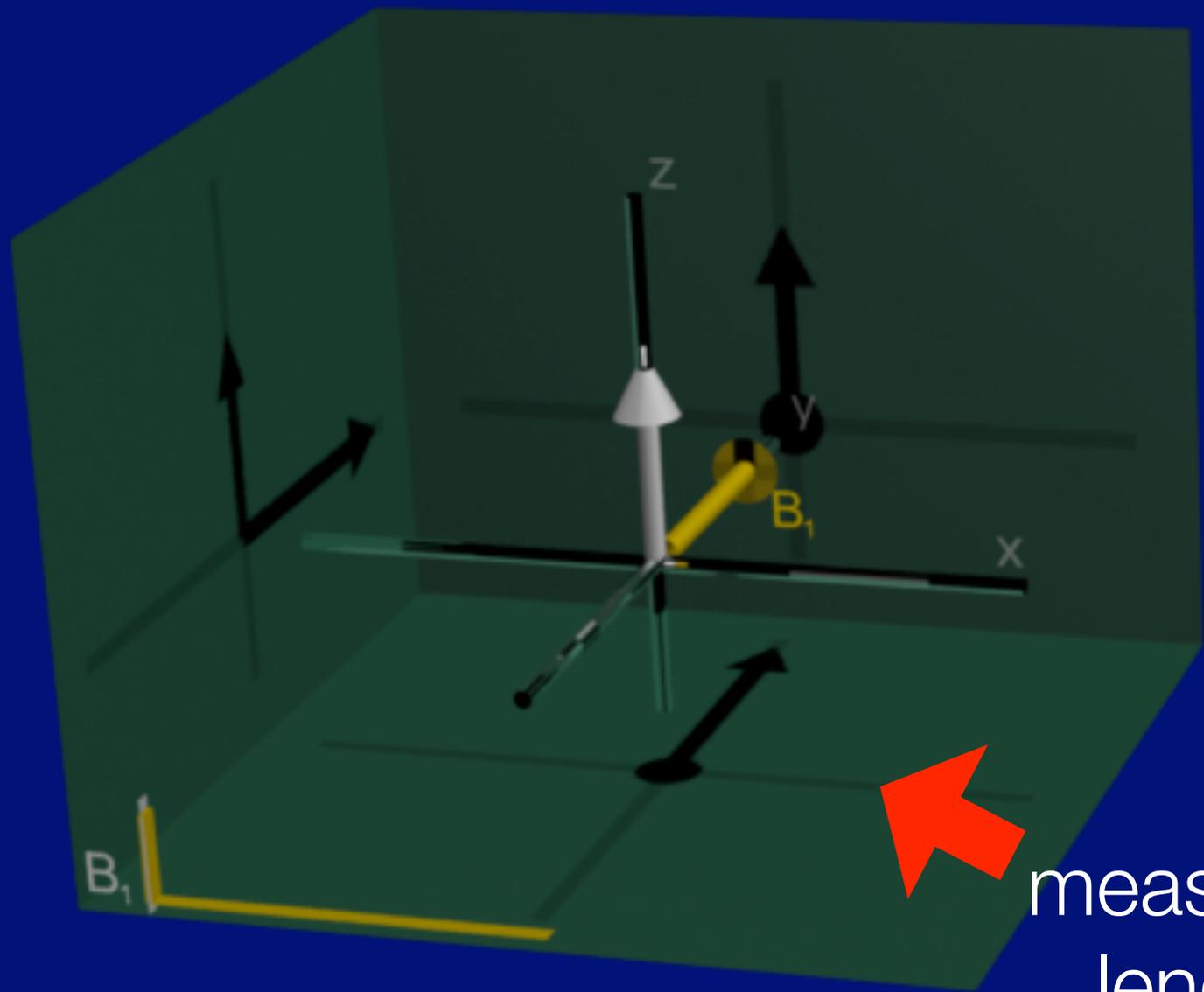


The **rate of precession**
changes **linearly** with the
strength of the **magnetic field**



main
magnetic
field





measured
length

“rotating frame of reference”



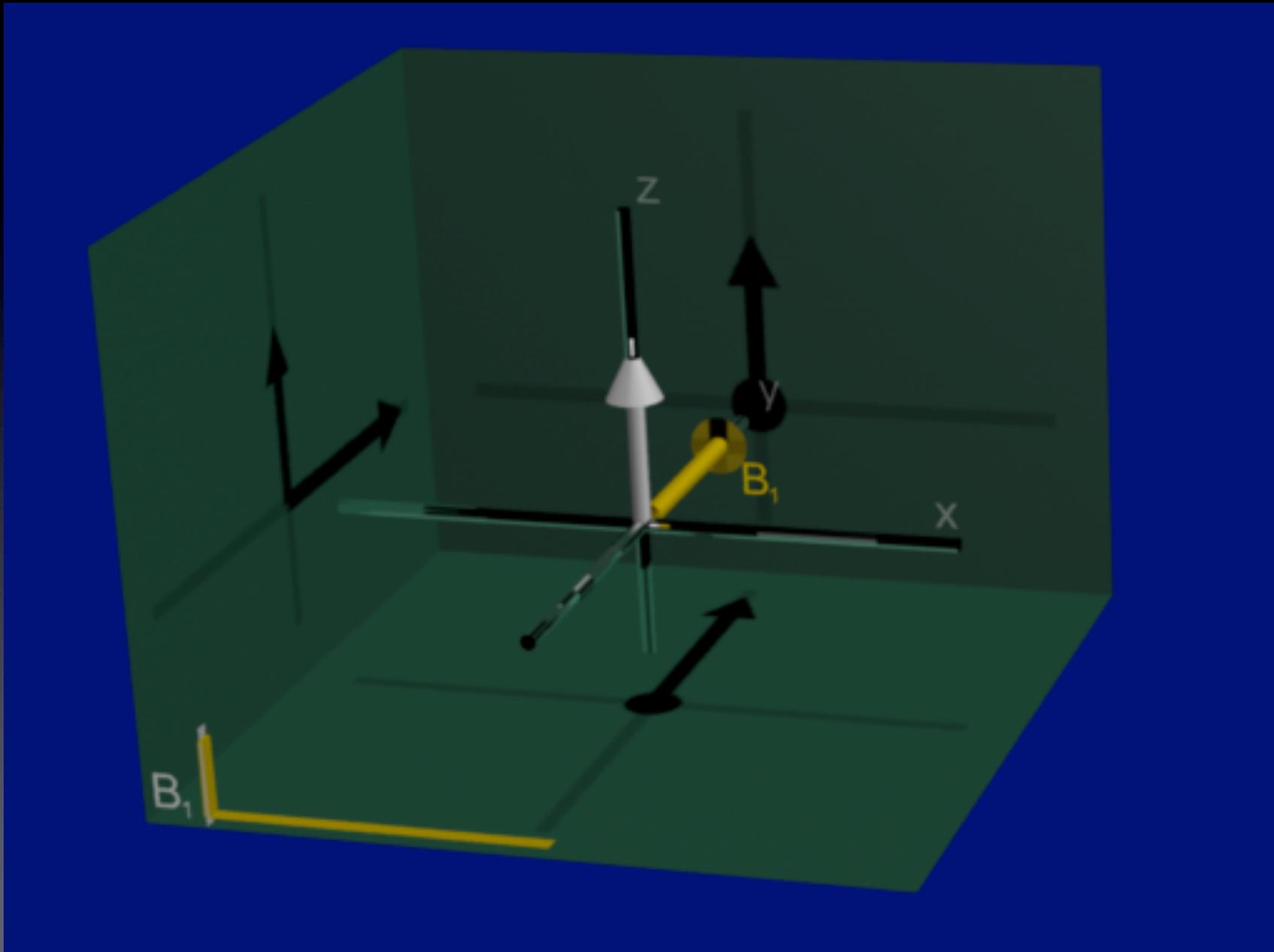
relaxation



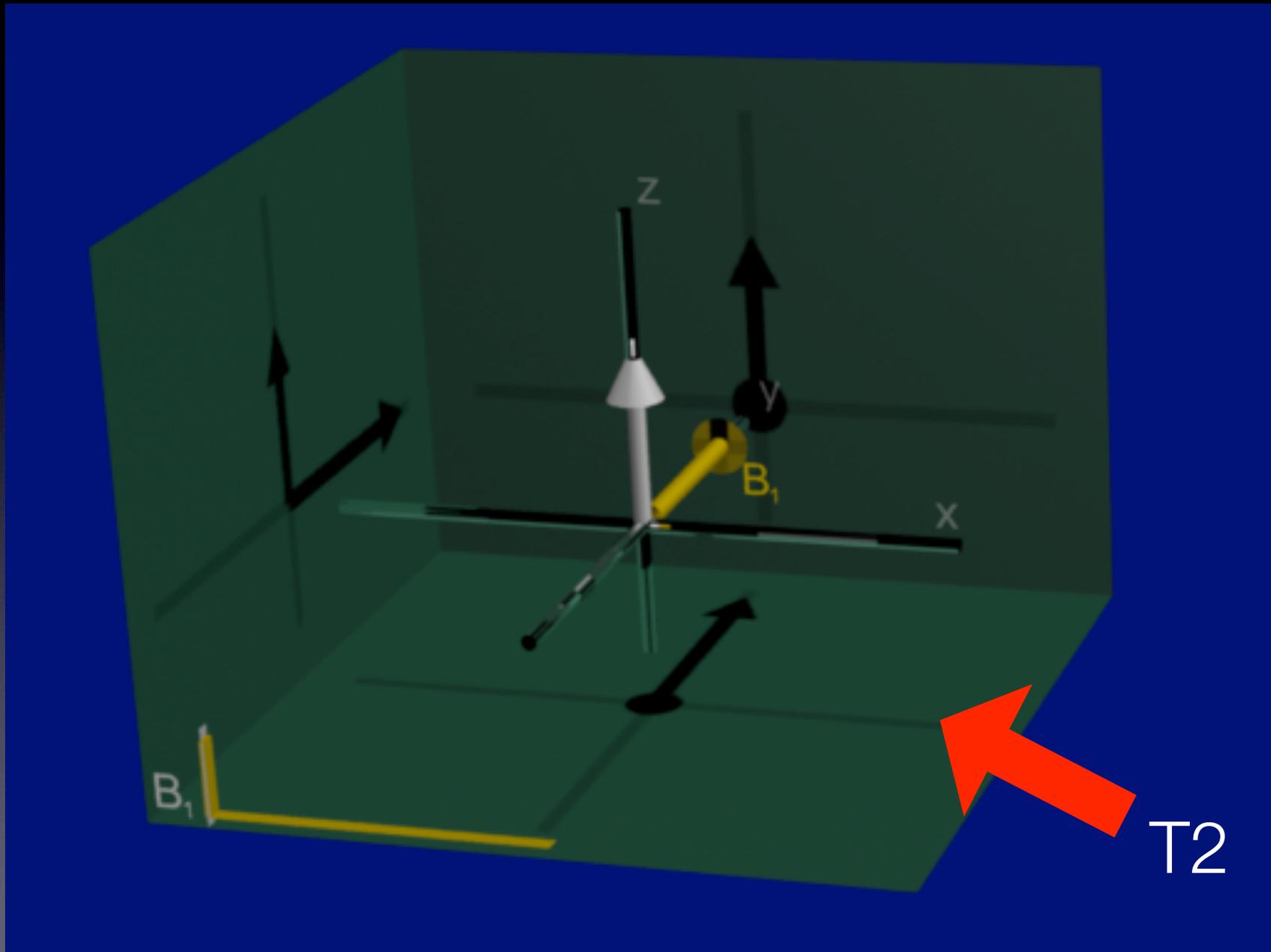
main
magnetic
field

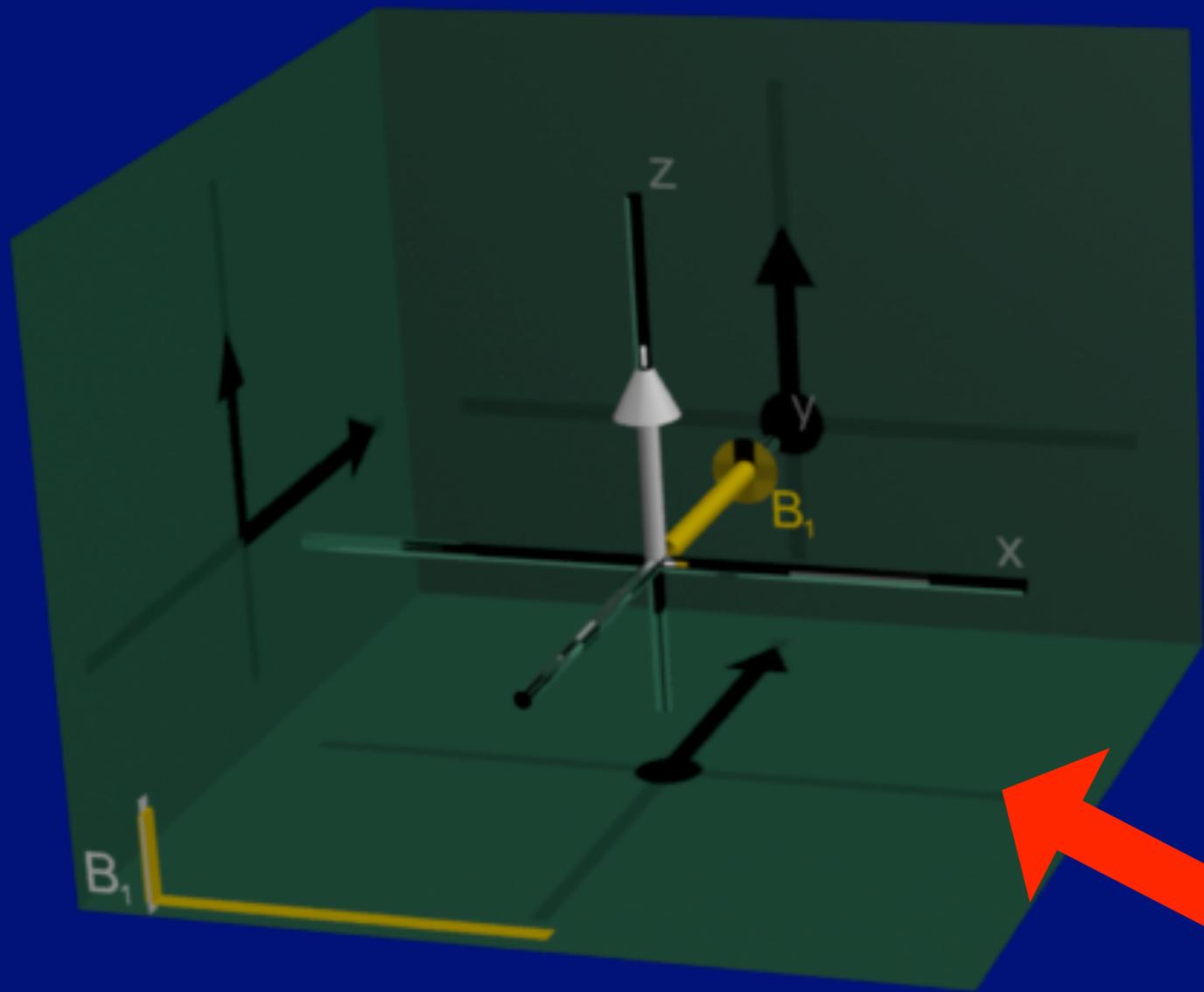


T2 is dephasing

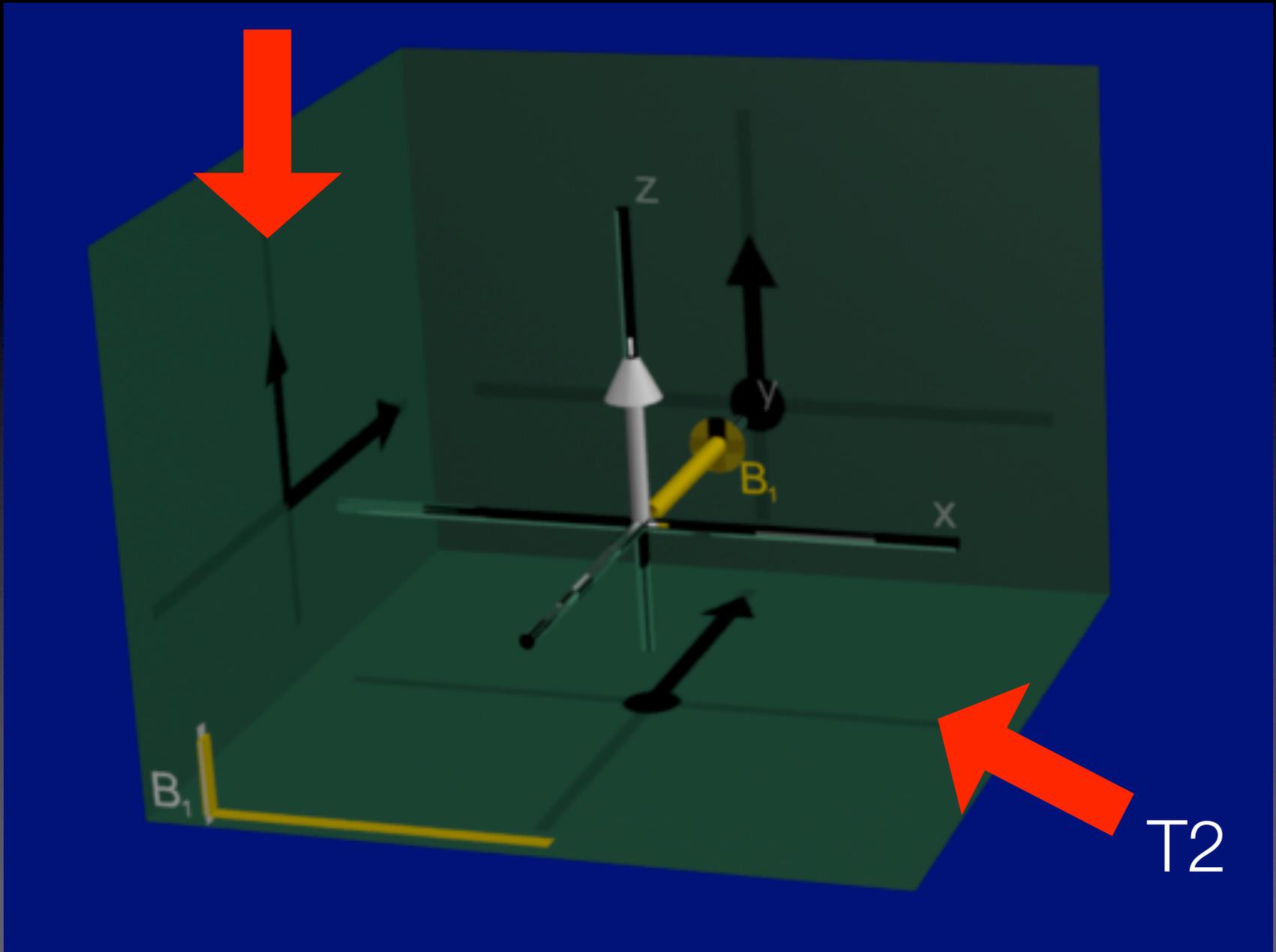


dephasing looks like “less signal”





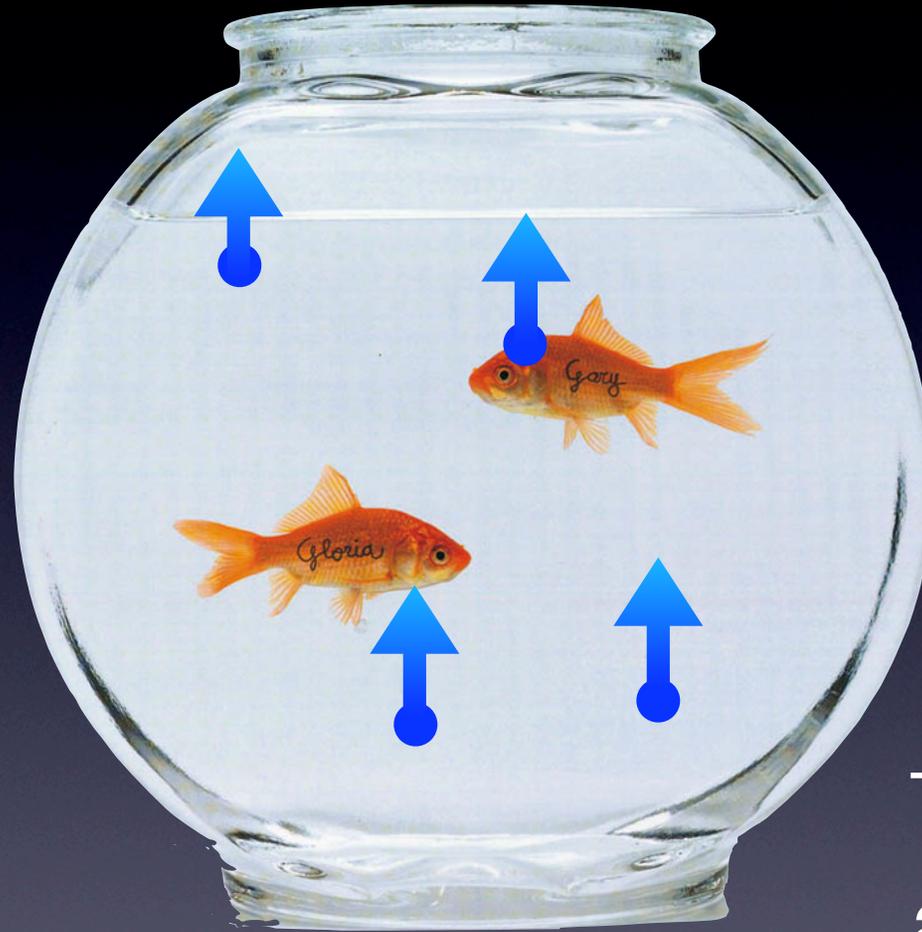
T1



T2

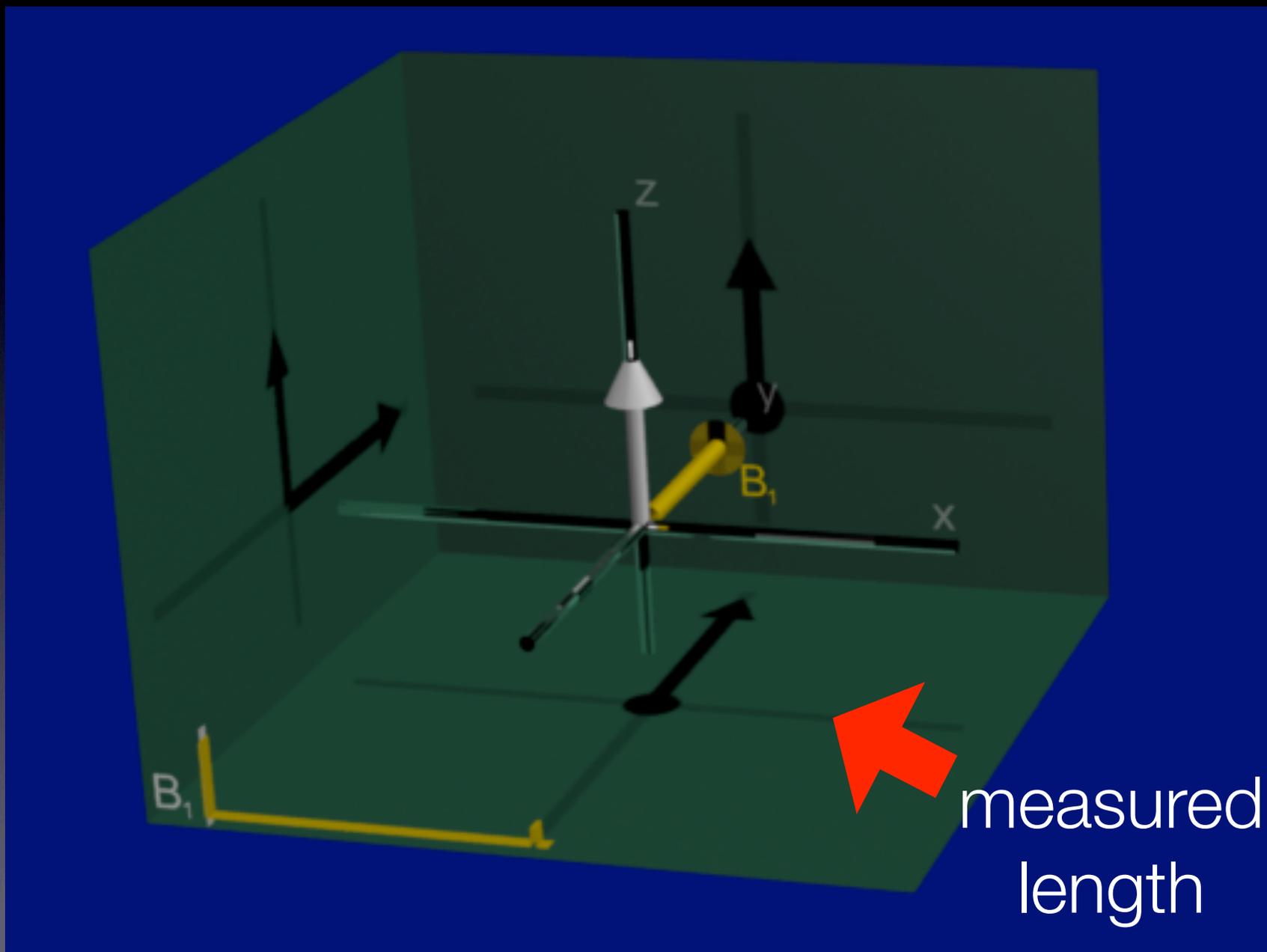


main
magnetic
field



The fish
are what
make it
interesting....

inversion recovery



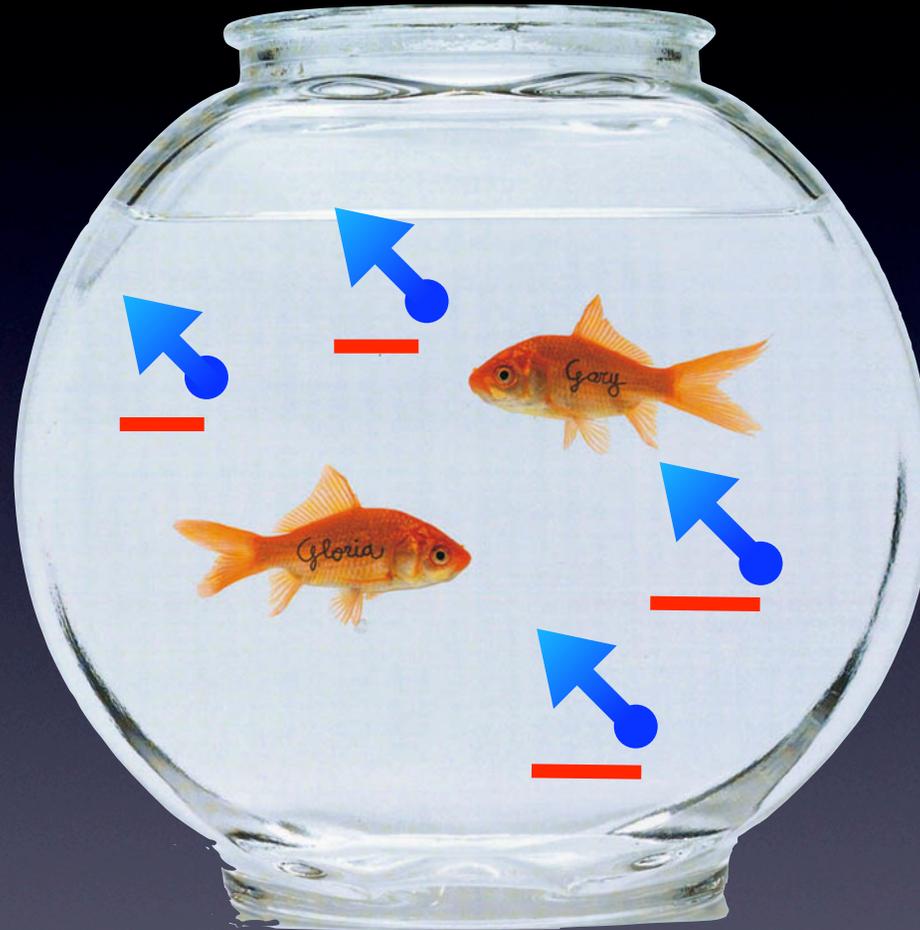
Using **inversion recovery** we
can **weight** our measurements
for tissues with **specific T1**

How do we get
spatial information?

what do we measure?

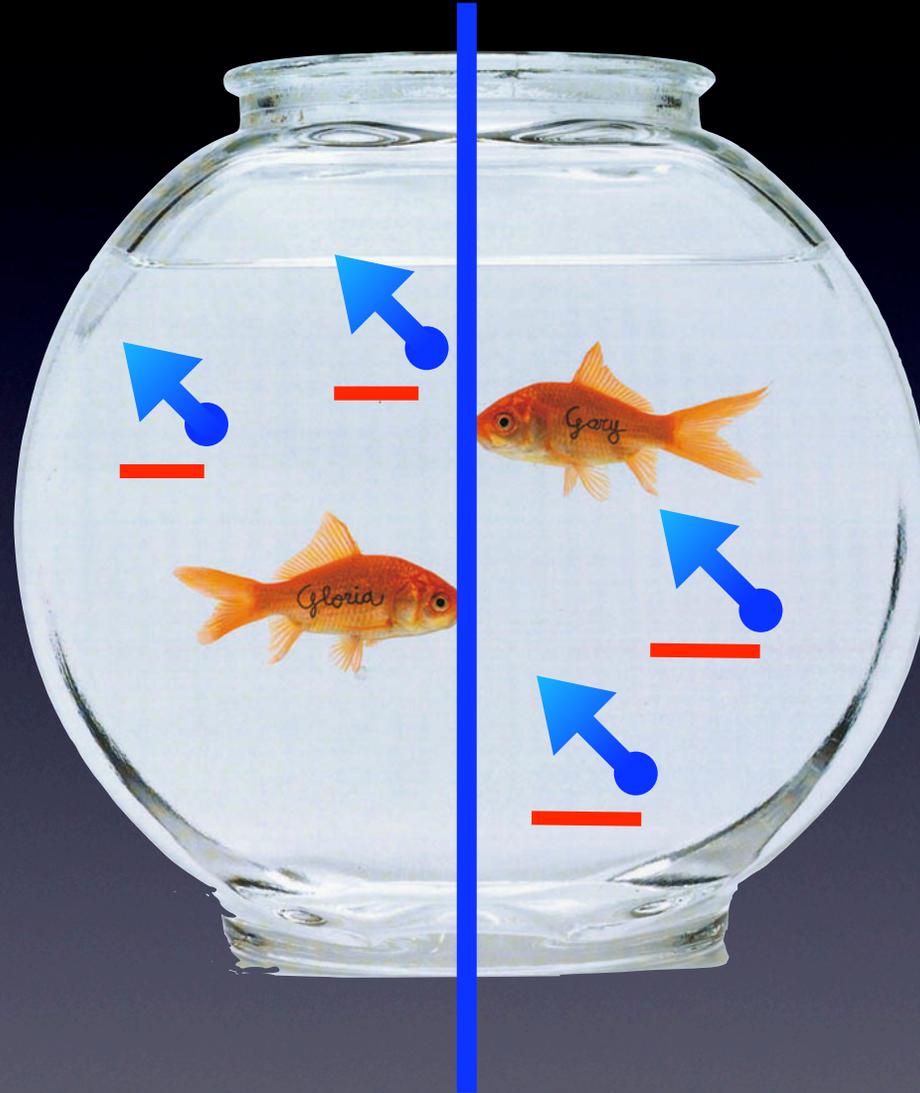


main
magnetic
field



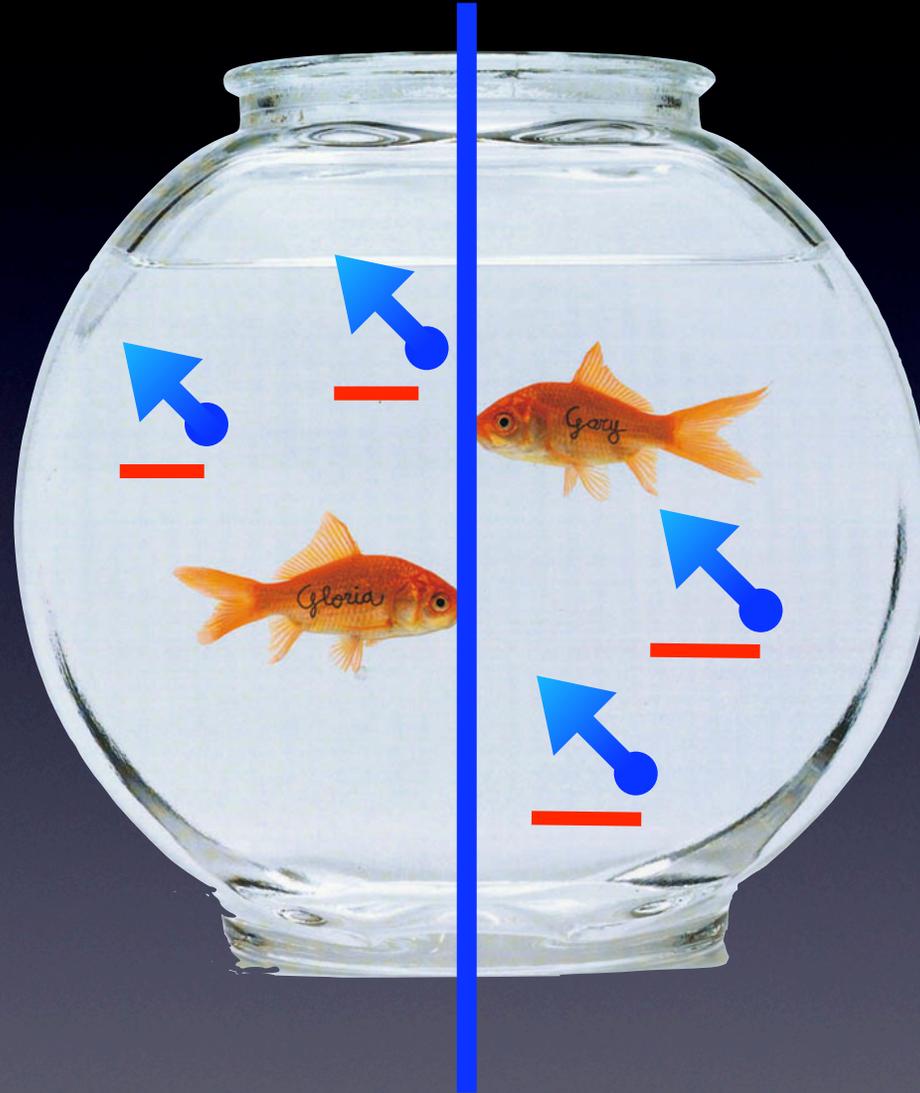
add up the red lines

two voxels (left and right)

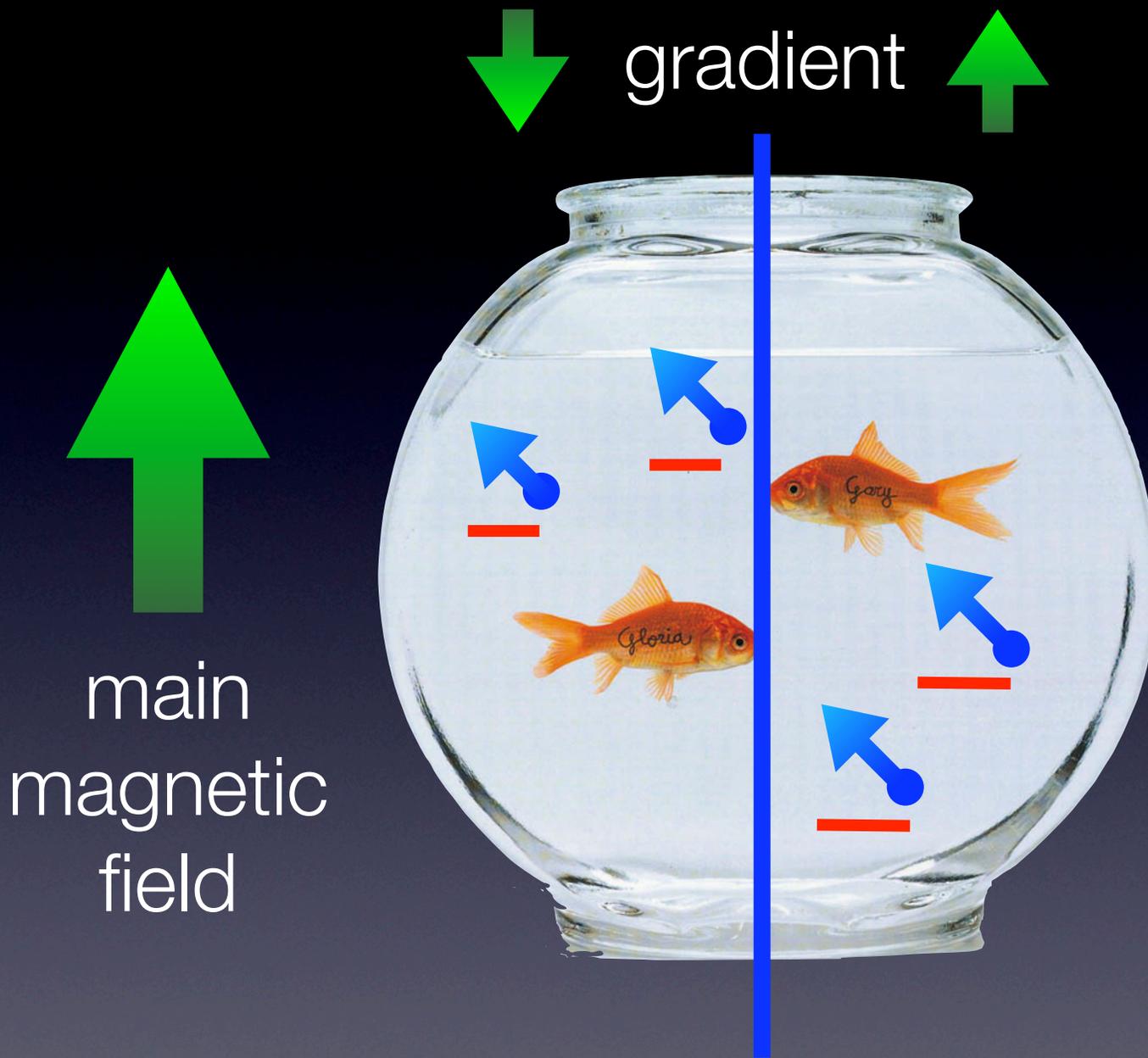


take one measurement (sum)

two voxels (left and right)



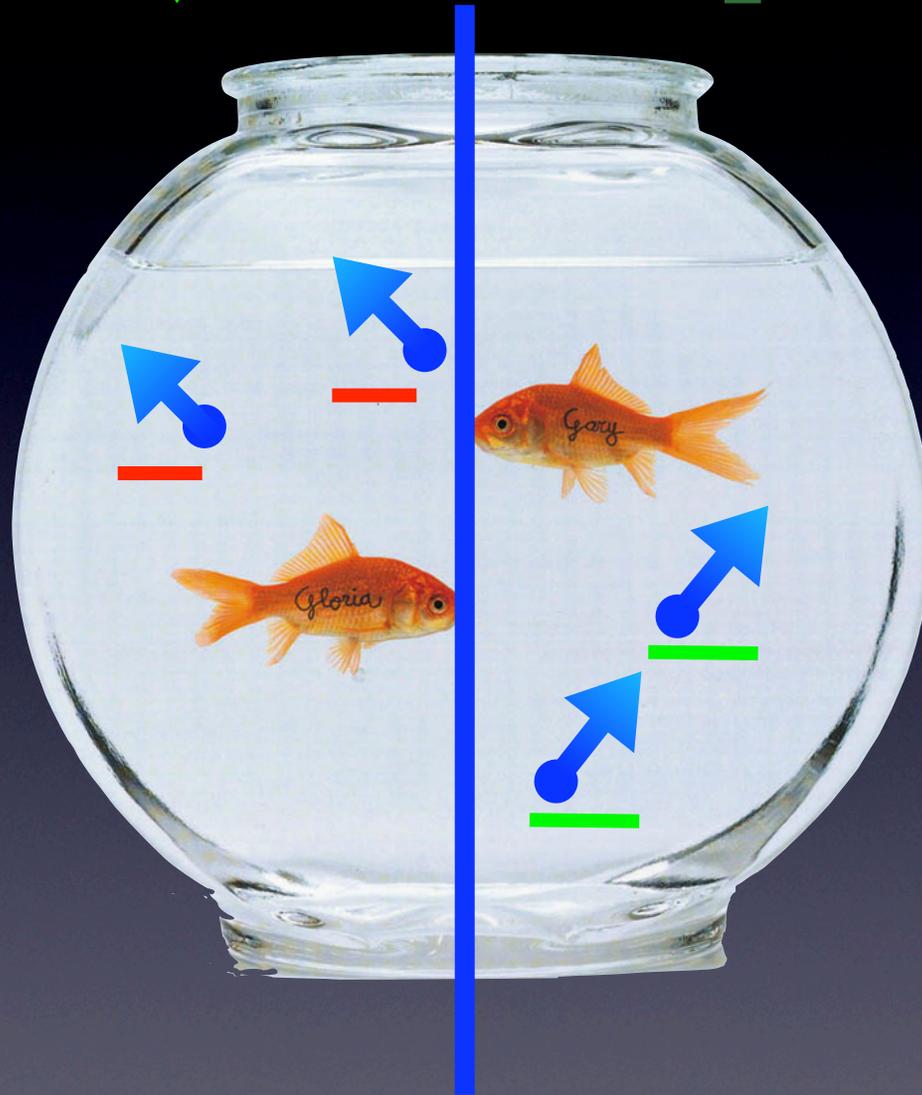
apply a different magnetic field to each half



apply a different magnetic field to each half

gradient

main
magnetic
field

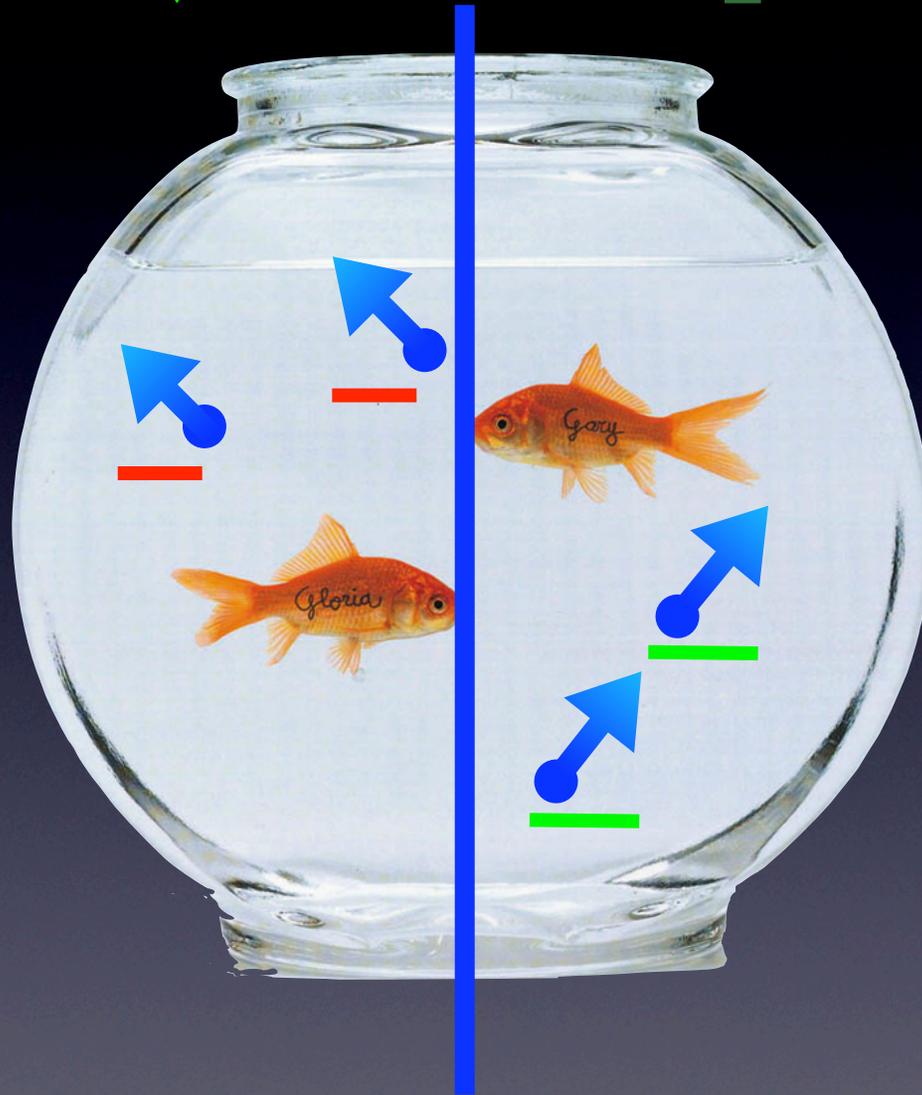


the voxels
are out of
phase

rate of precession is different in each voxel

gradient

main
magnetic
field



the voxels
are out of
phase

take second measurement (sum)

1st measurement: left + right

2nd measurement: left - right

1st measurement: left + right

2nd measurement: left - right

add them: 2 x left

1st measurement: left + right

2nd measurement: left - right

subtract them: 2 x right

Real sequences sum together fractional amounts from all the voxels.

The fractions are changed using the x-, y-, or z-gradients.

The voxels are “unmixed” from all the measurements using an Inverse Fourier Transform.

A Pulse Sequence

1. “Prepare” (invert, flip)

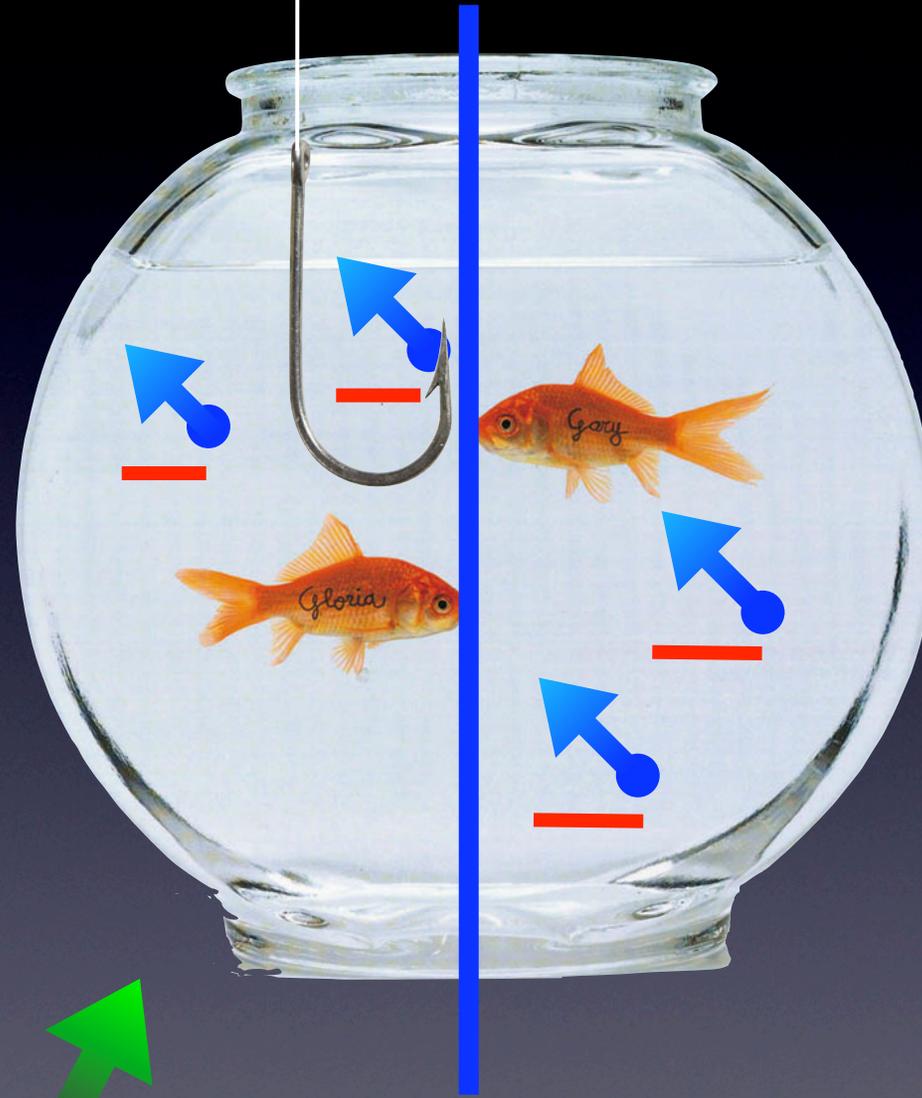
2. Localize (Gradients)

3. Measure repeat

4. Relax

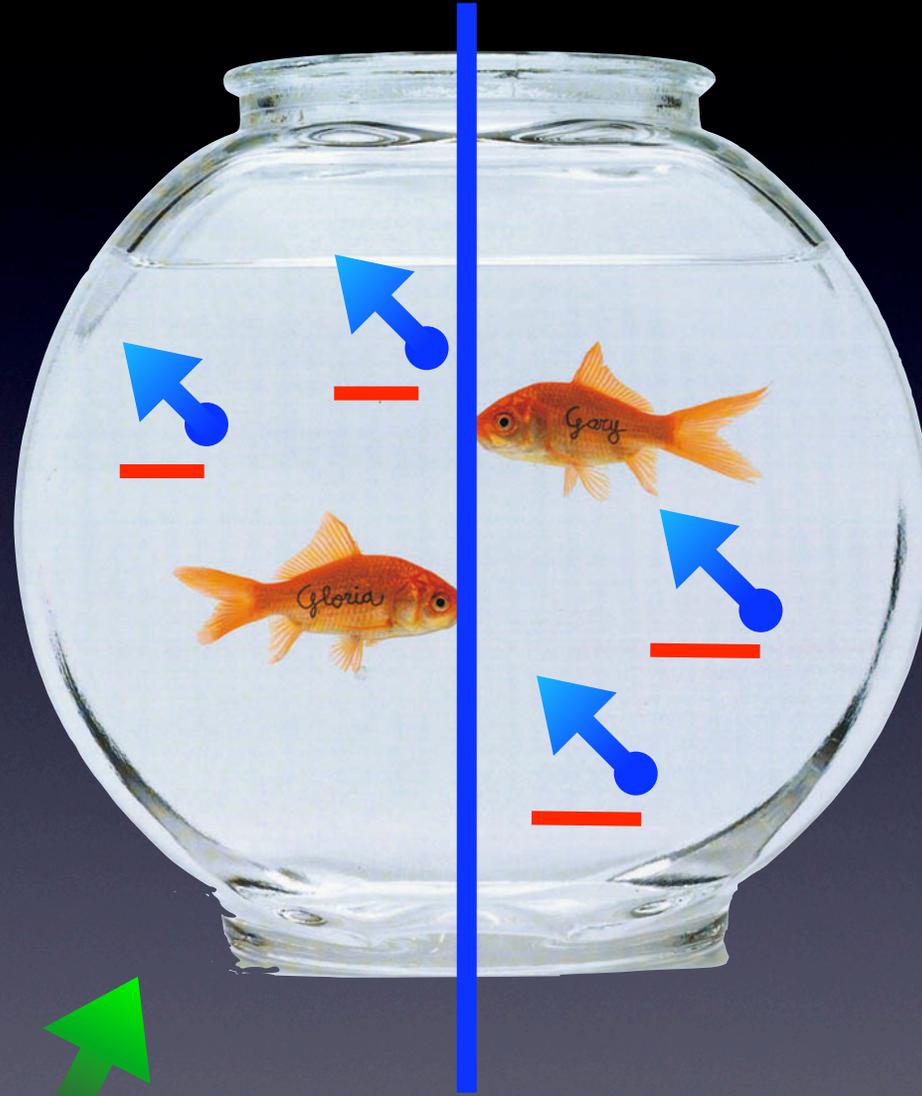
5. Go back to 1.

fMRI (BOLD)



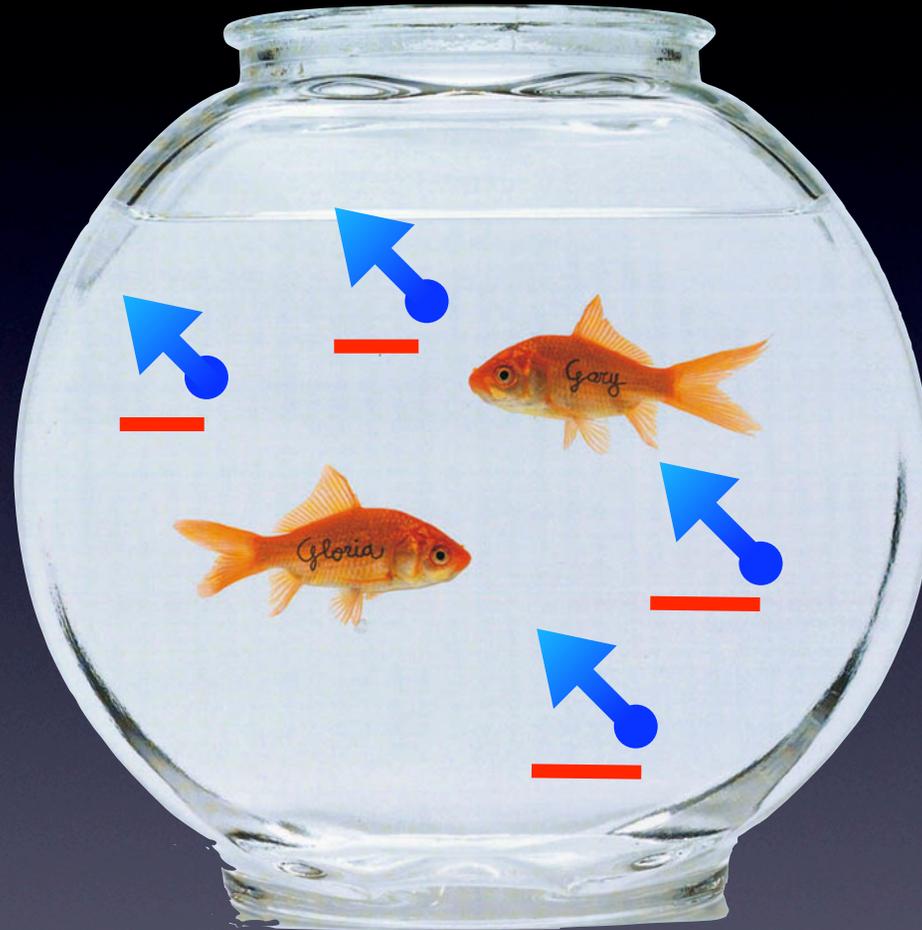
this side dephases faster = less signal

fMRI (BOLD)

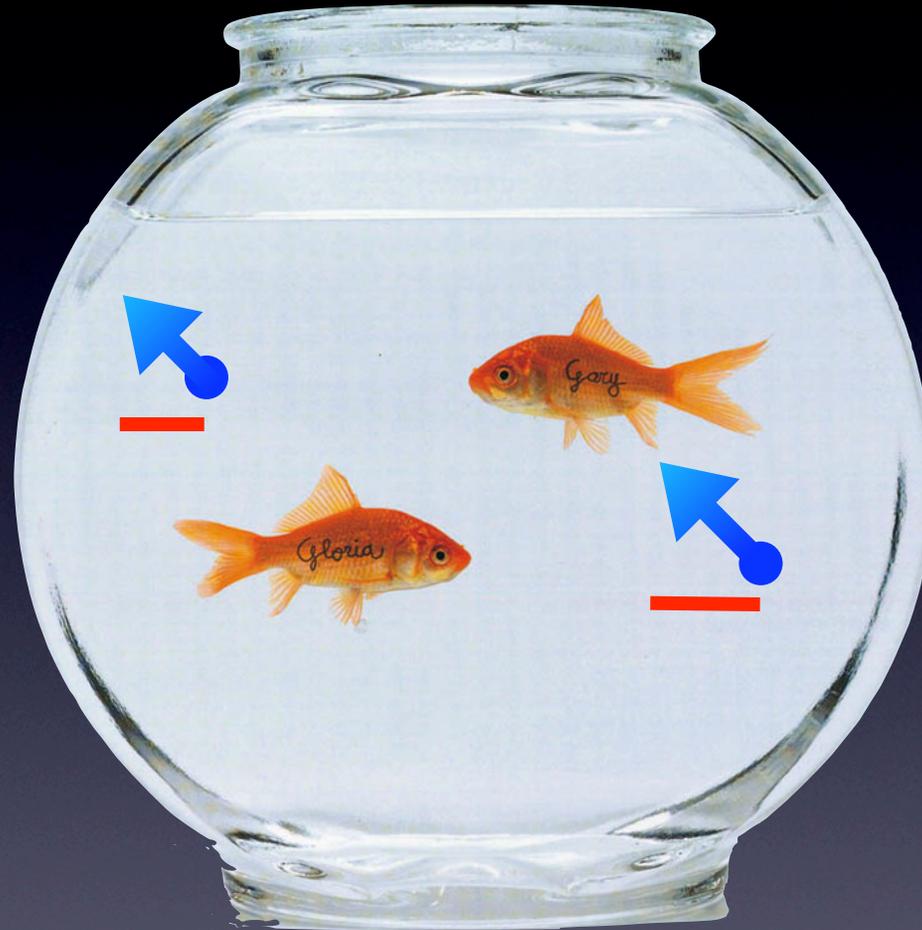


this side's T2 returns to normal

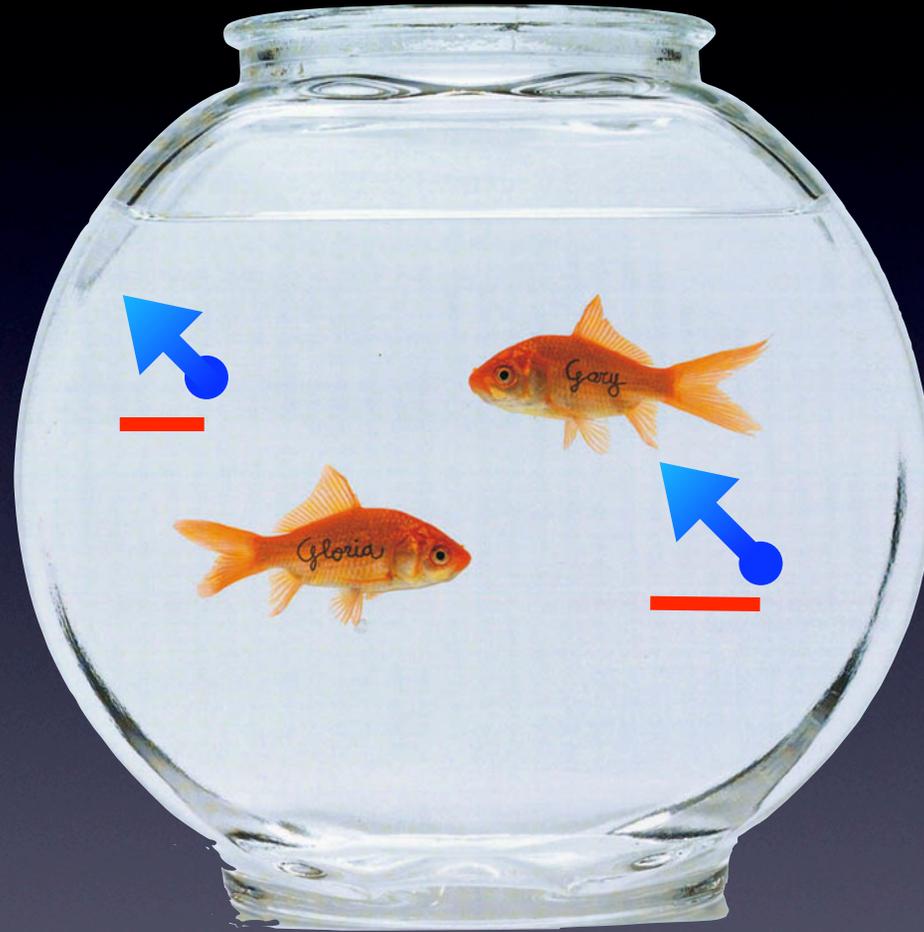
Diffusion



Diffusion

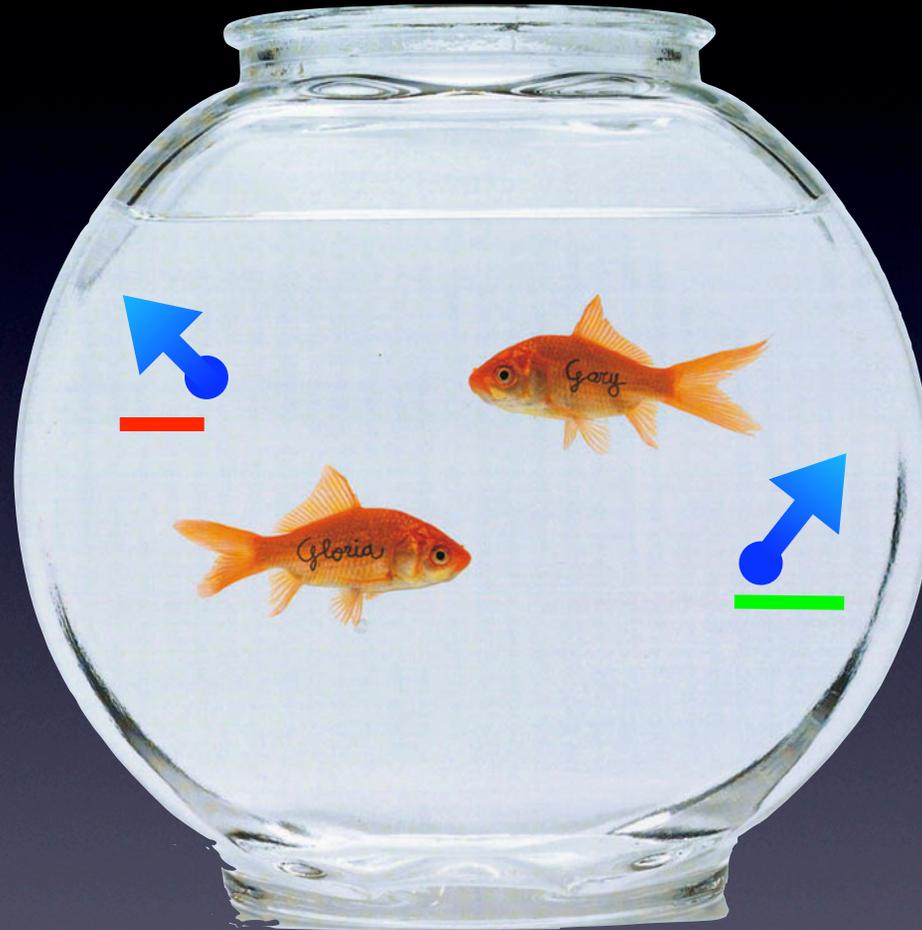


Diffusion



gradient

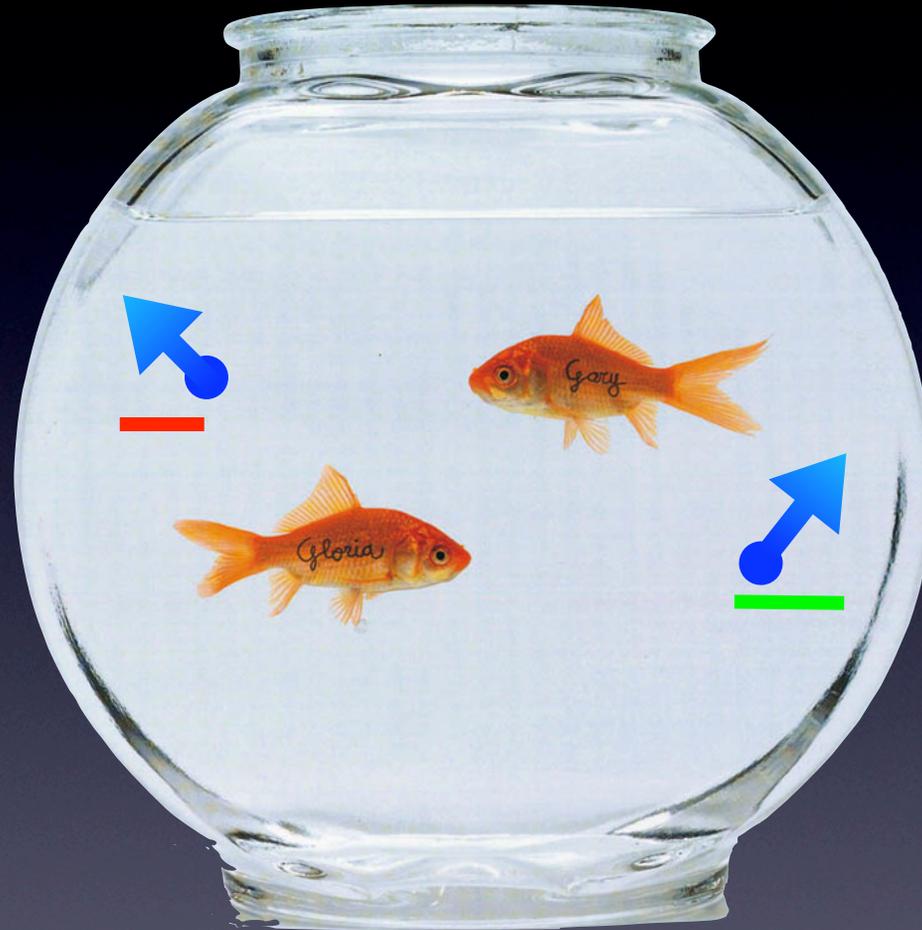
Diffusion



gradient

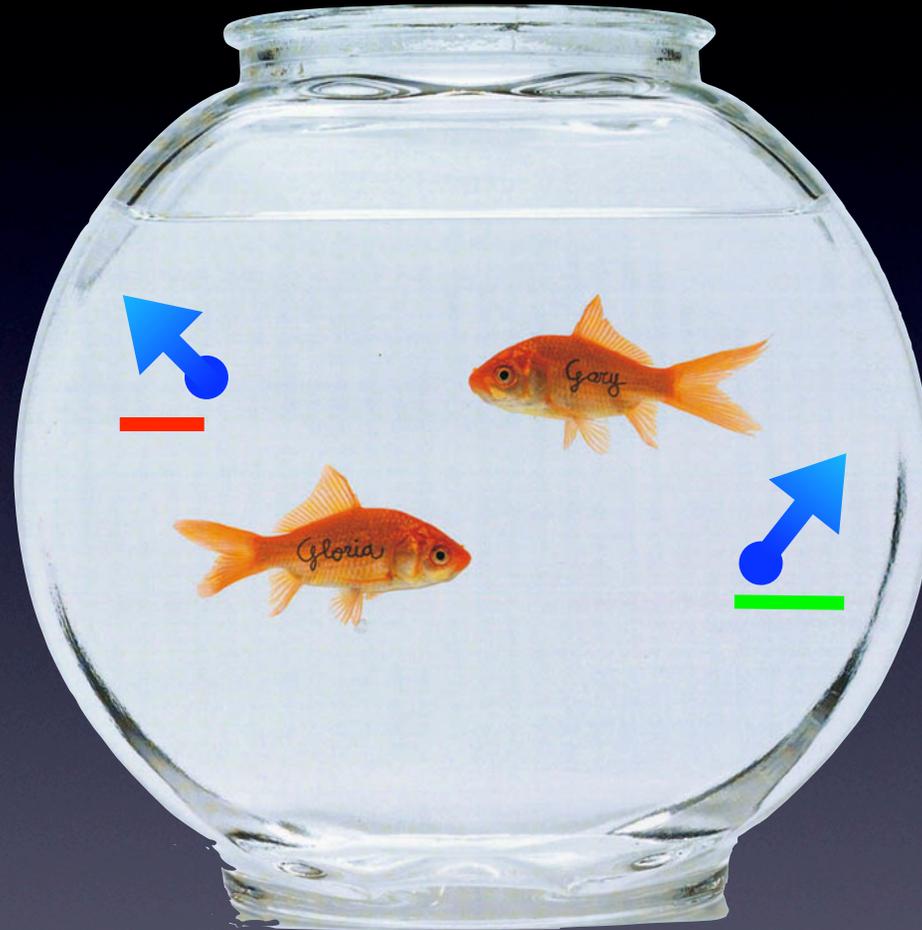


Diffusion



no gradient

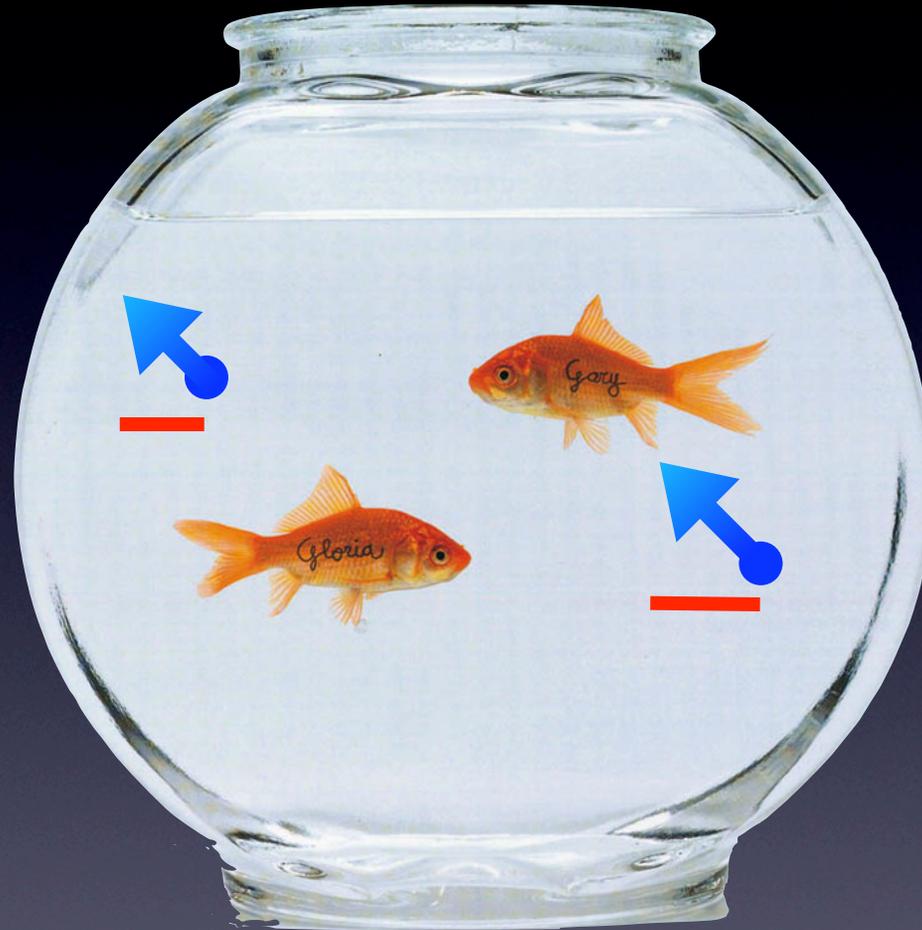
Diffusion



opposite
gradient



Diffusion



opposite
gradient

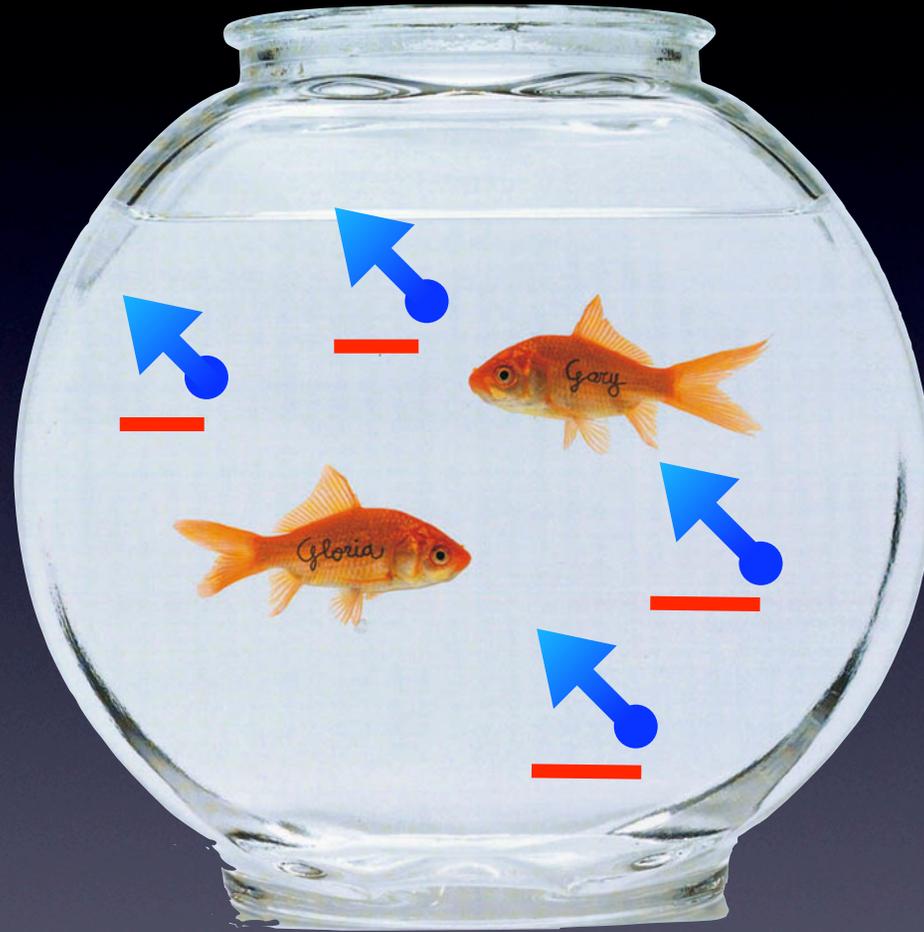


Water molecules diffuse (move) inside of all tissues.

At 37 C, water diffuse has diffusion rate of $3 \times 10^{-3} \text{ mm}^2/\text{s}$.

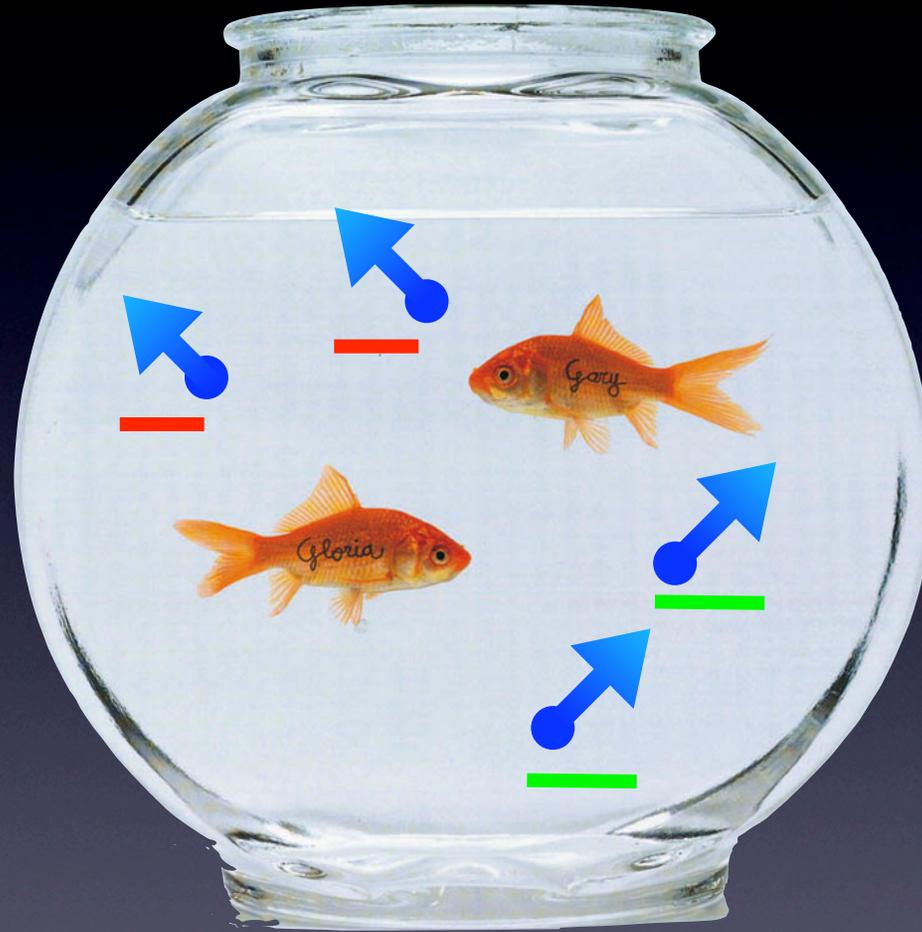
We expect a displacement of about $17 \text{ }\mu\text{m}$ in 50 ms

Diffusion



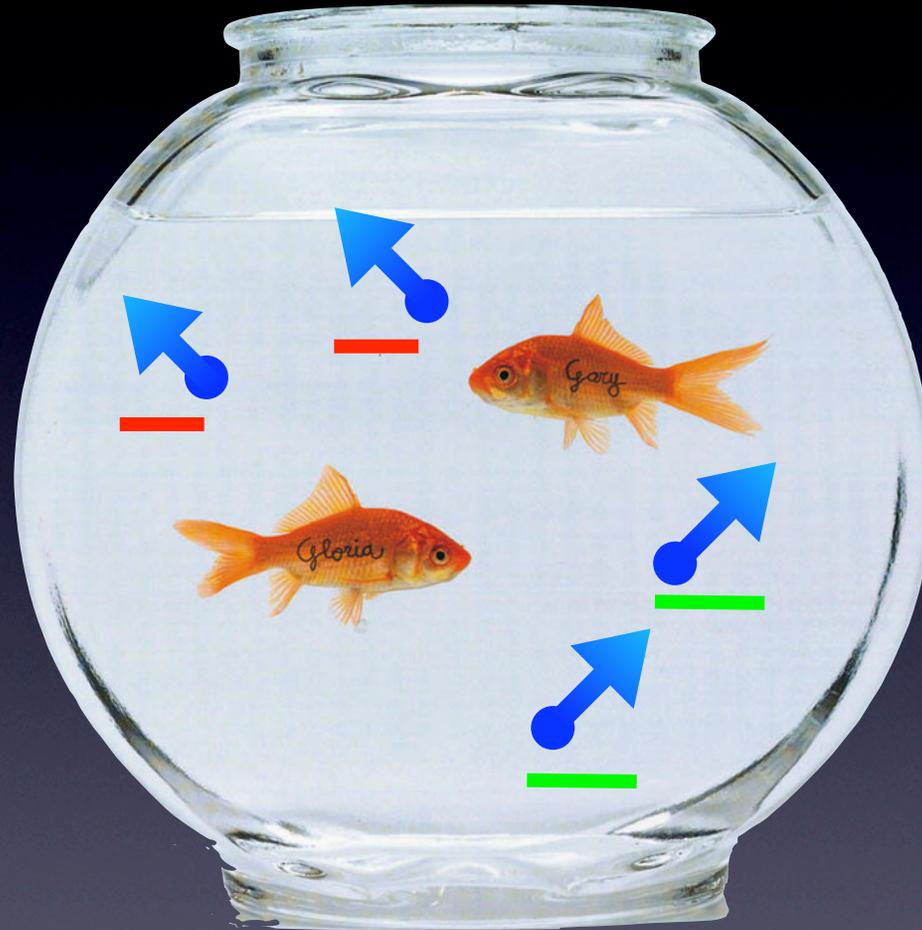
gradient

Diffusion



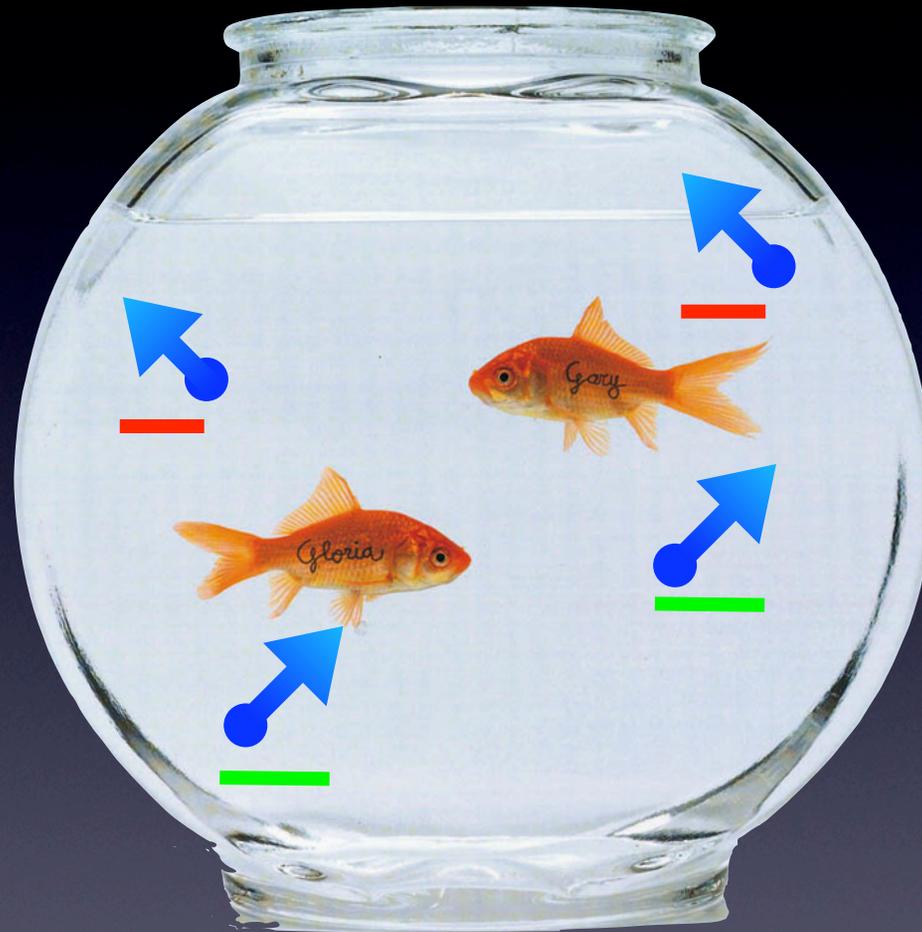
gradient

Diffusion



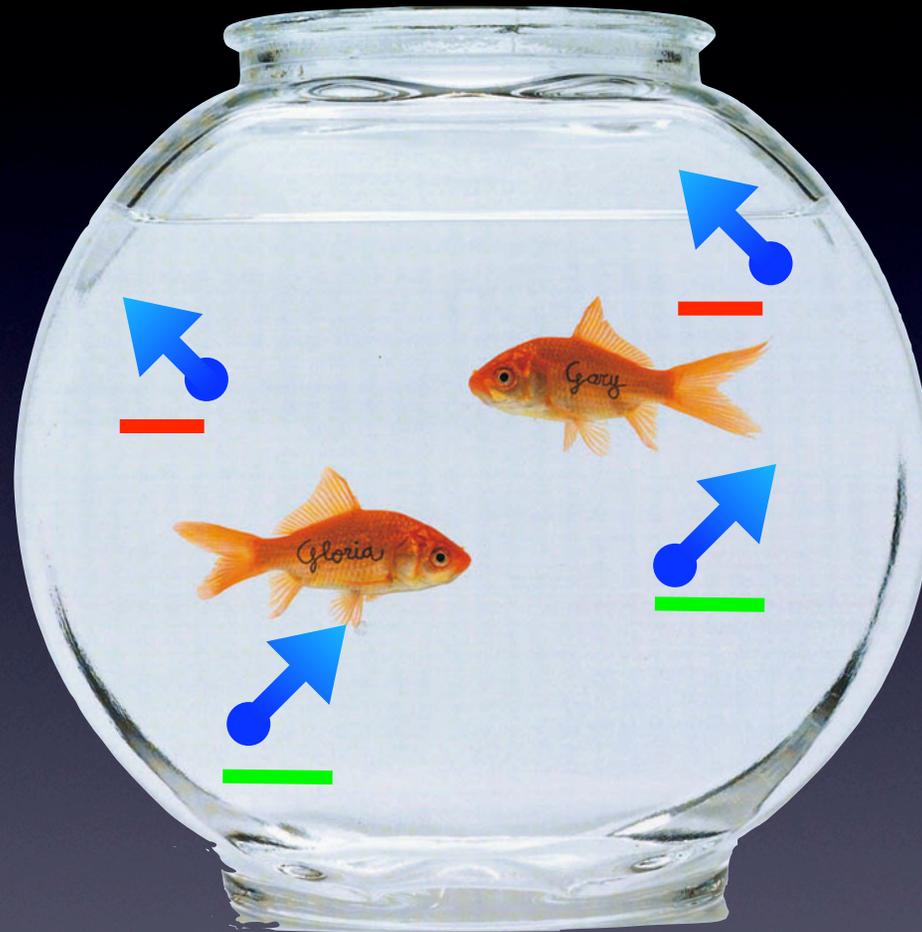
no gradient

Diffusion



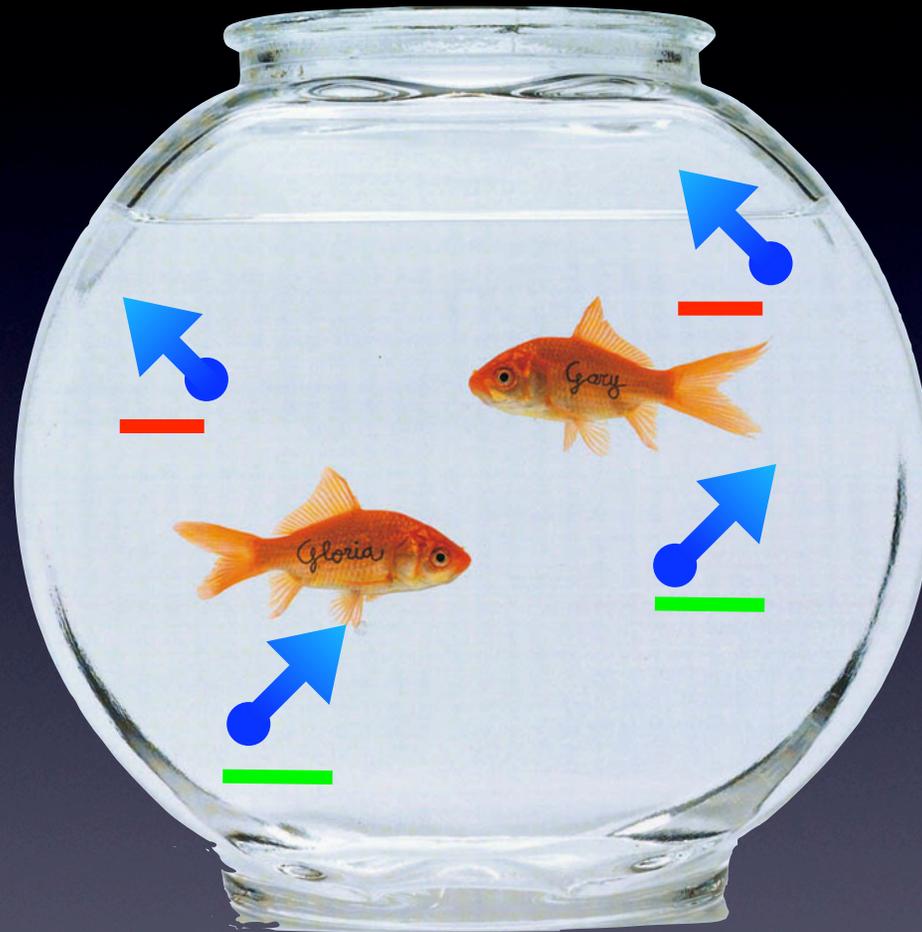
no gradient

Diffusion



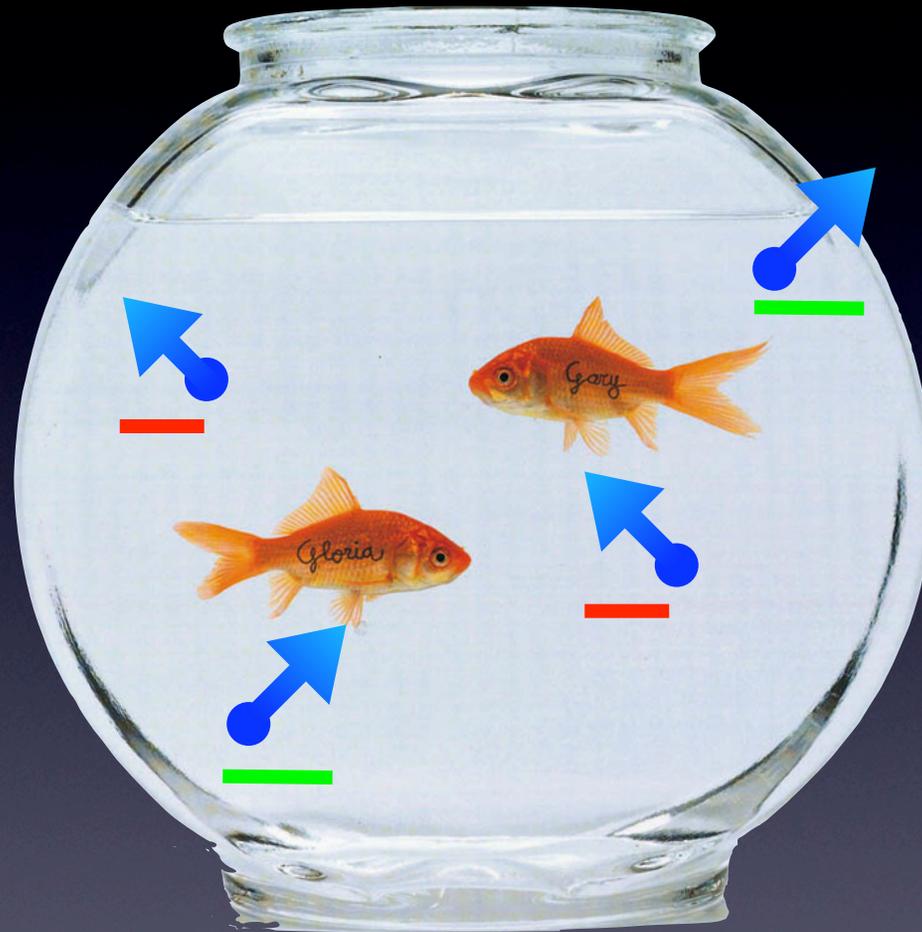
no gradient

Diffusion



opposite
gradient

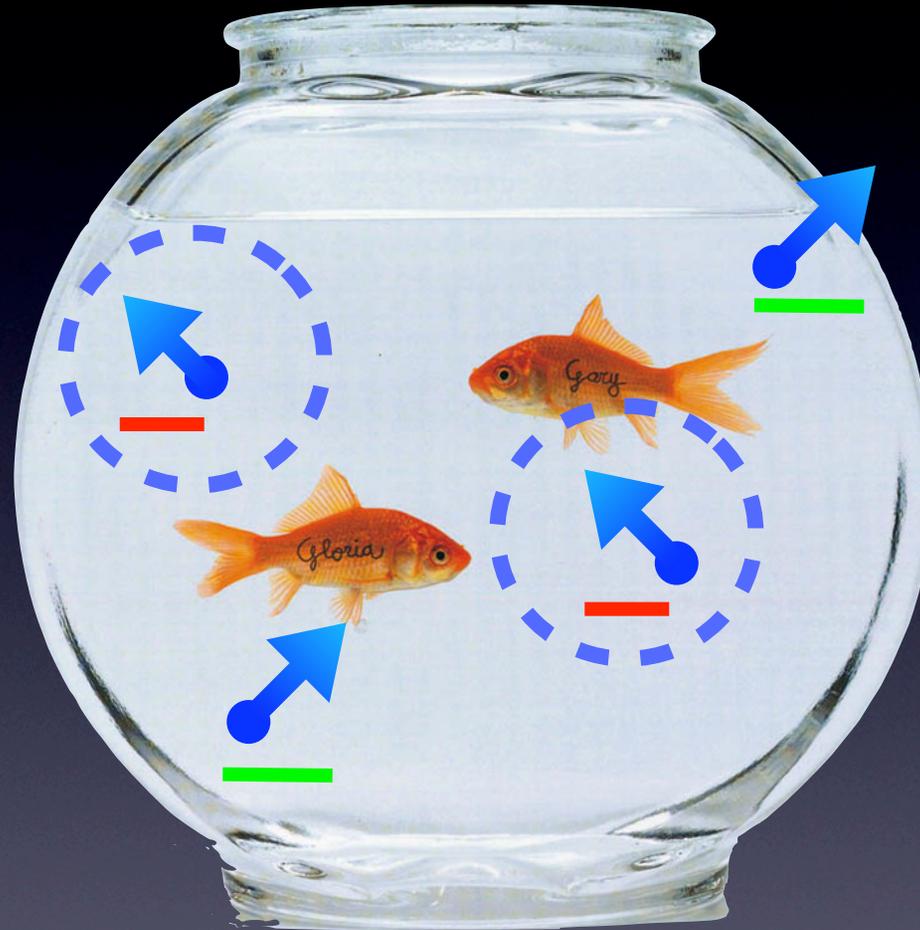
Diffusion



opposite
gradient

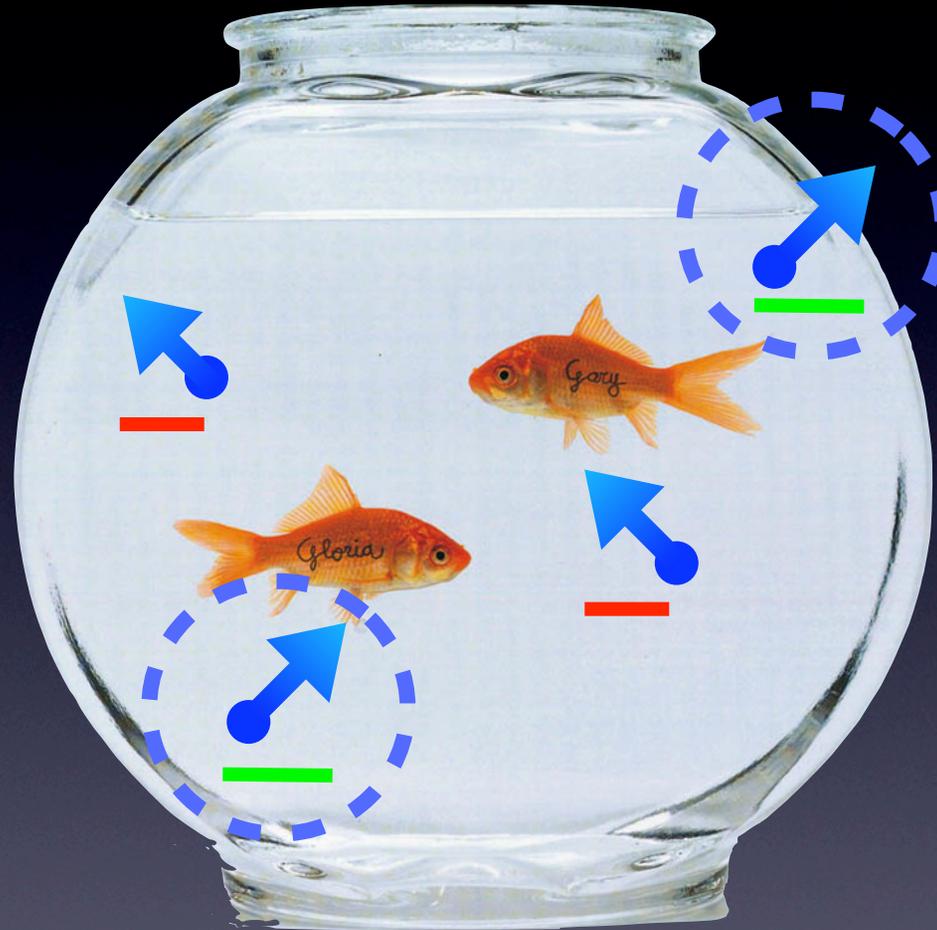
Diffusion

stationary =
re-focused



opposite
gradient

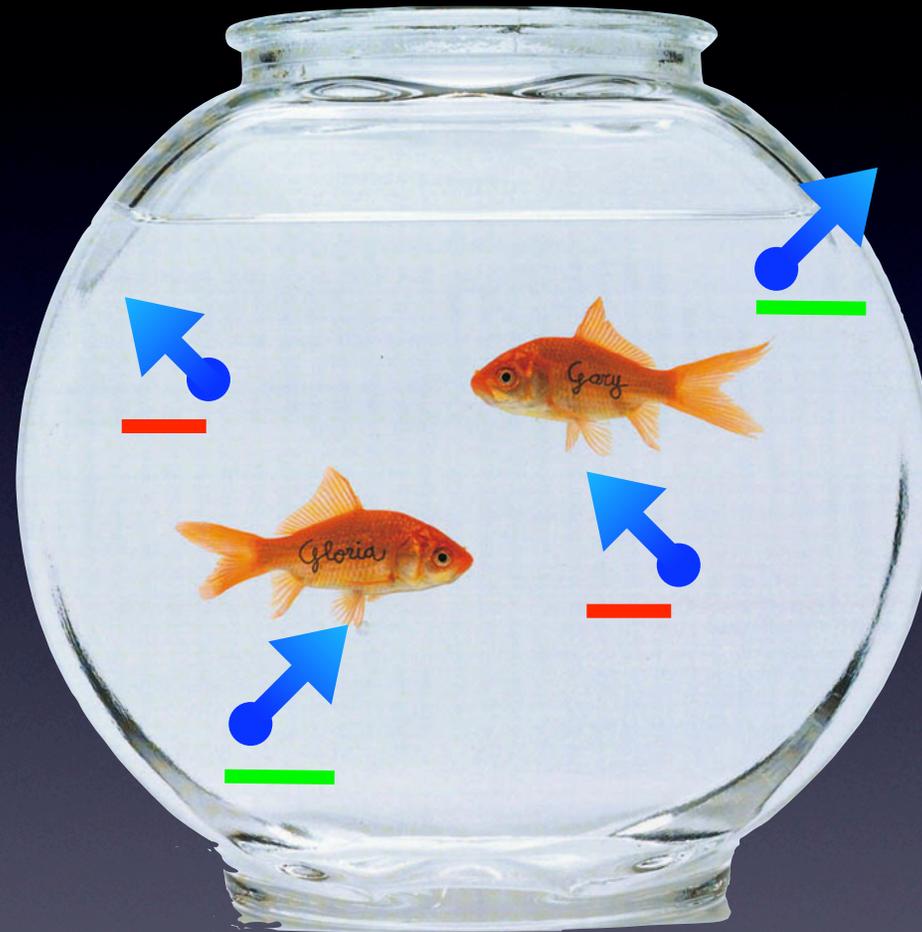
Diffusion



diffused =
not
re-focused

opposite
gradient

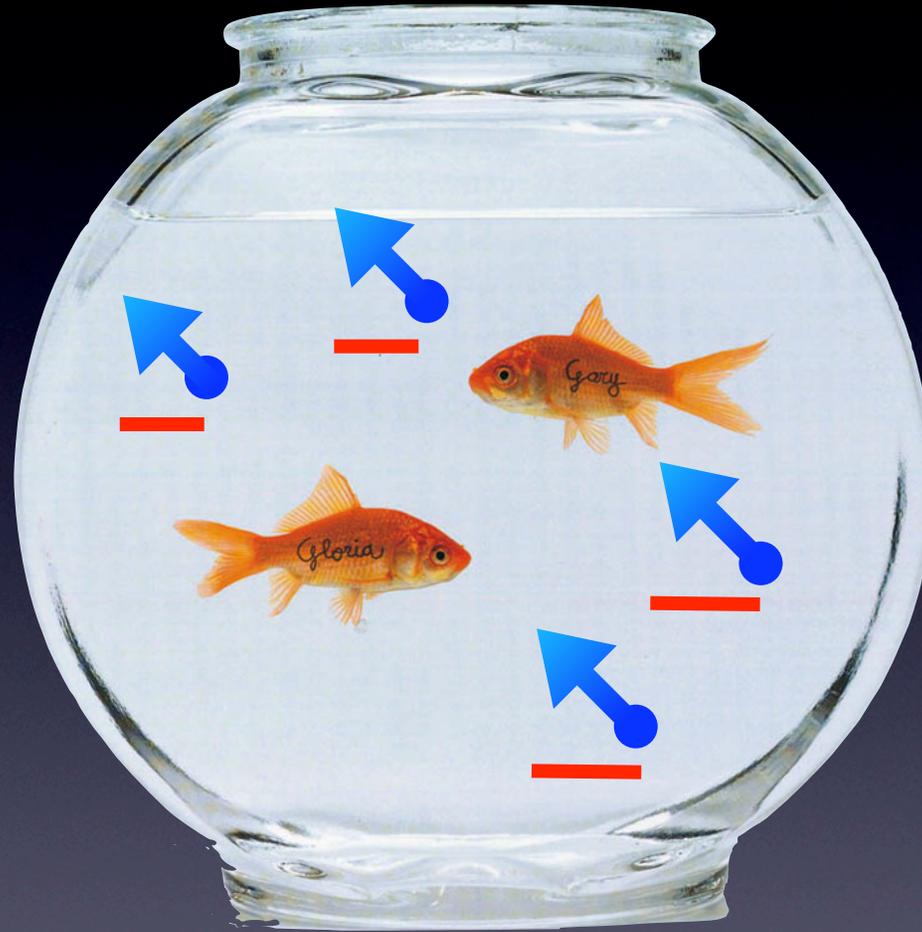
Diffusion



signal has cancelled out because of
diffusion parallel to the gradients

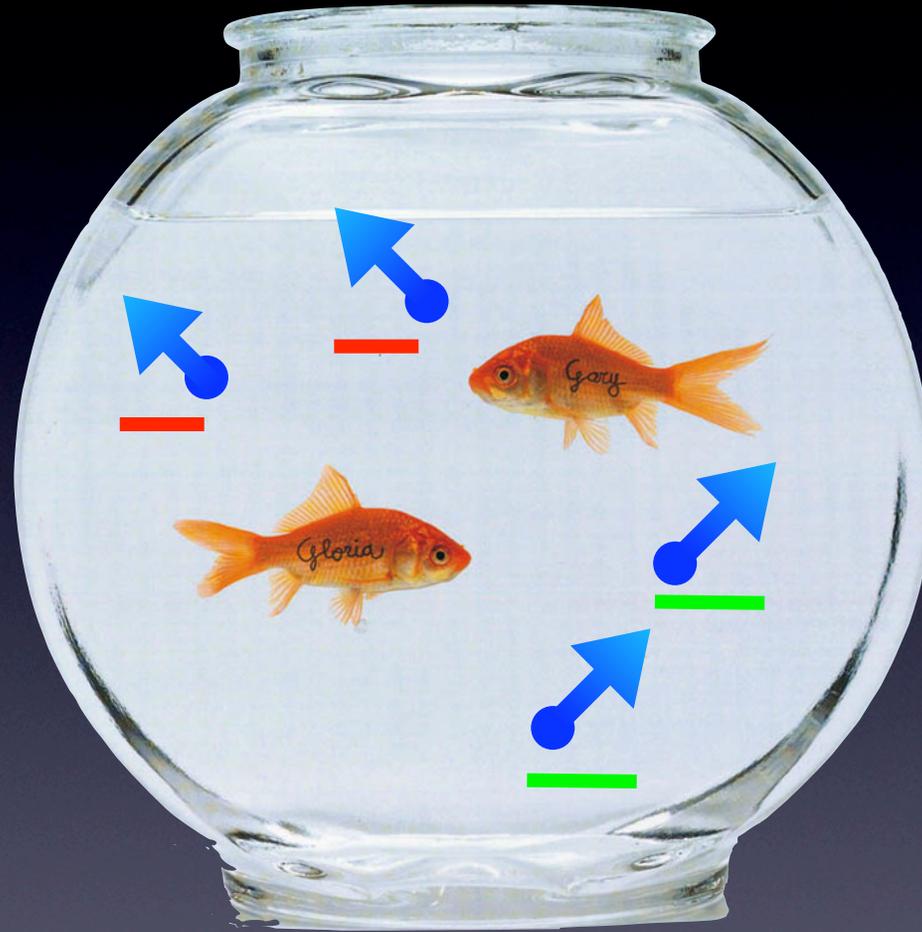
What happens with diffusion perpendicular to the gradients?

Diffusion



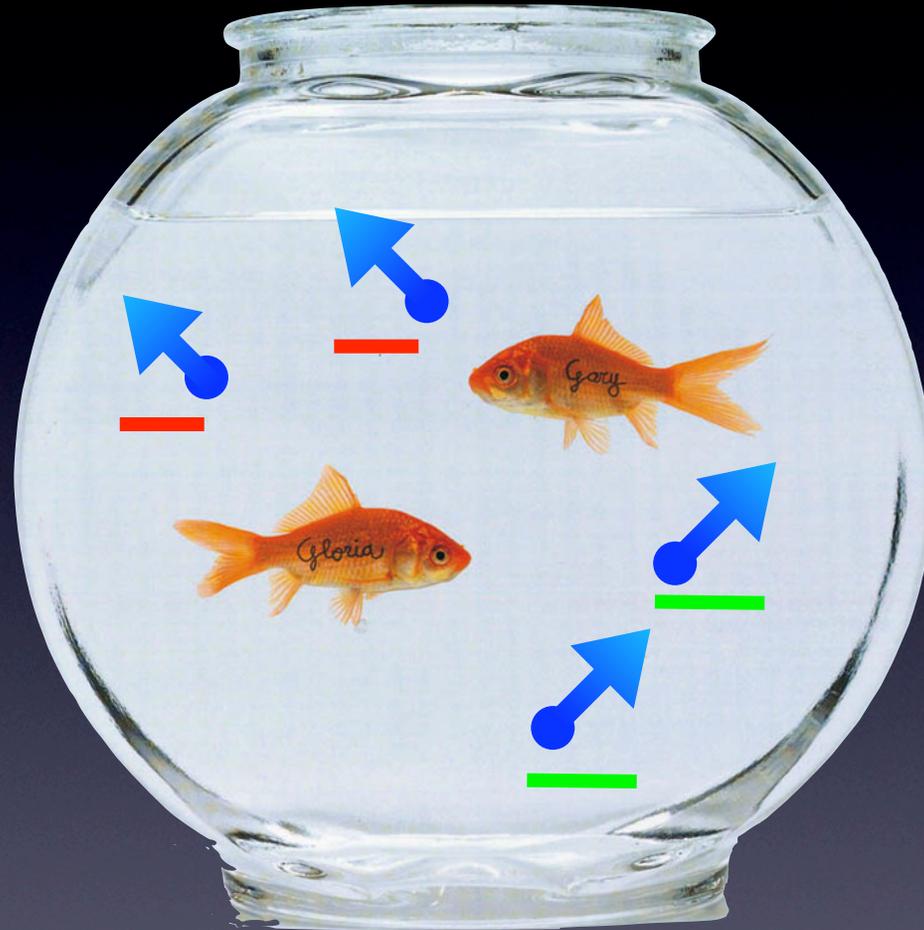
gradient

Diffusion



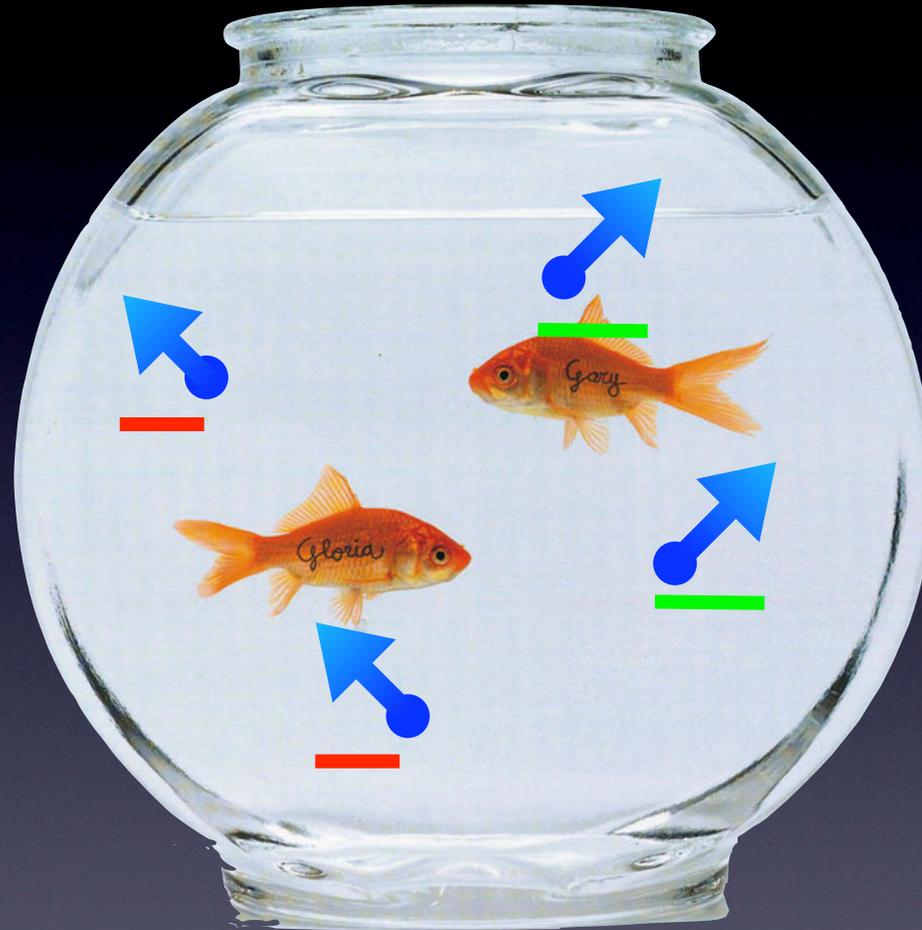
gradient

Diffusion



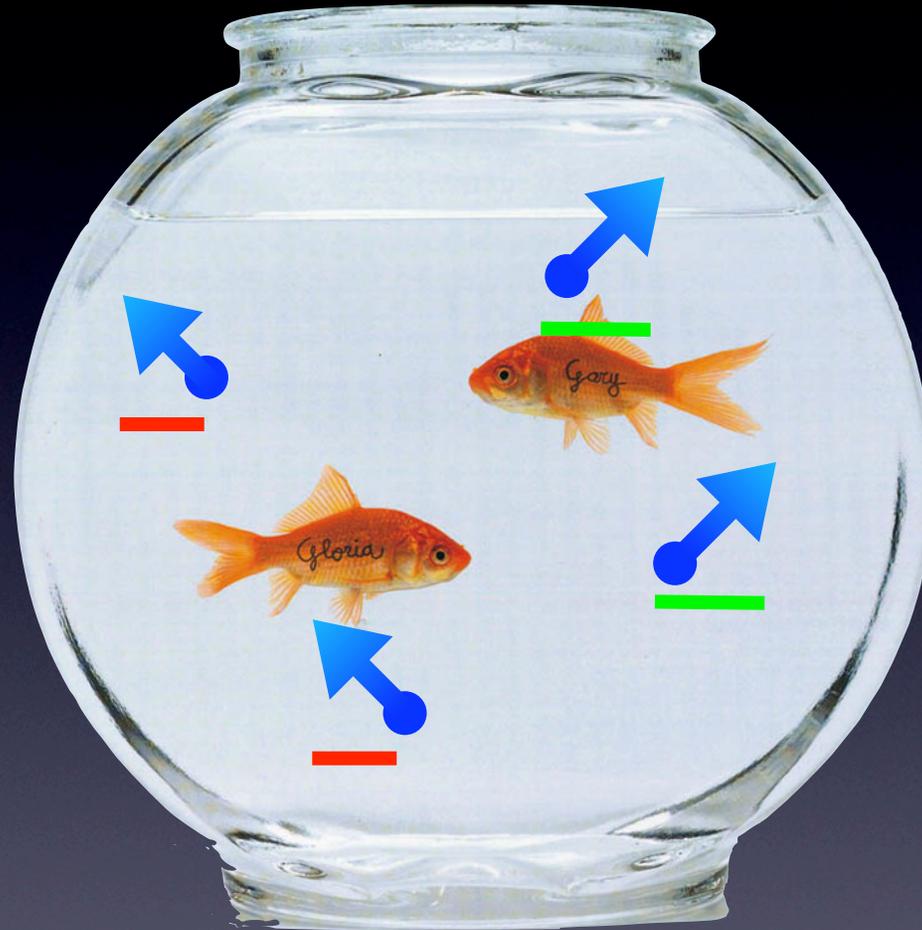
no gradient

Diffusion



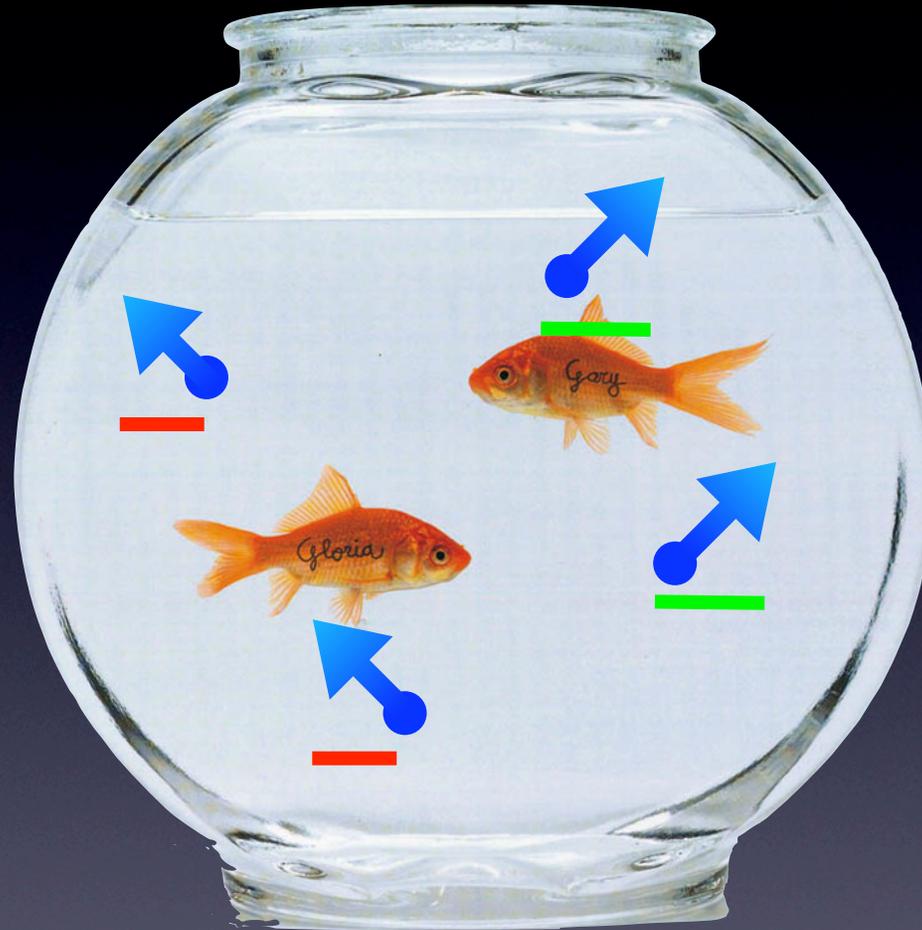
no gradient

Diffusion



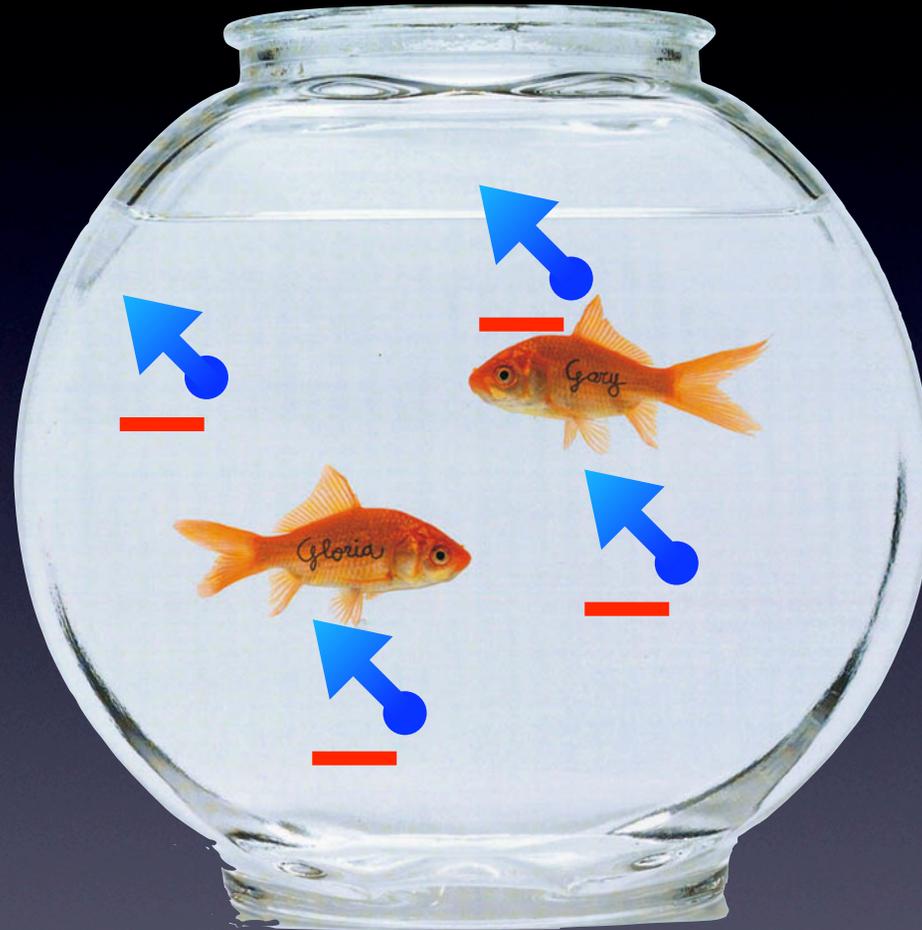
no gradient

Diffusion



opposite
gradient

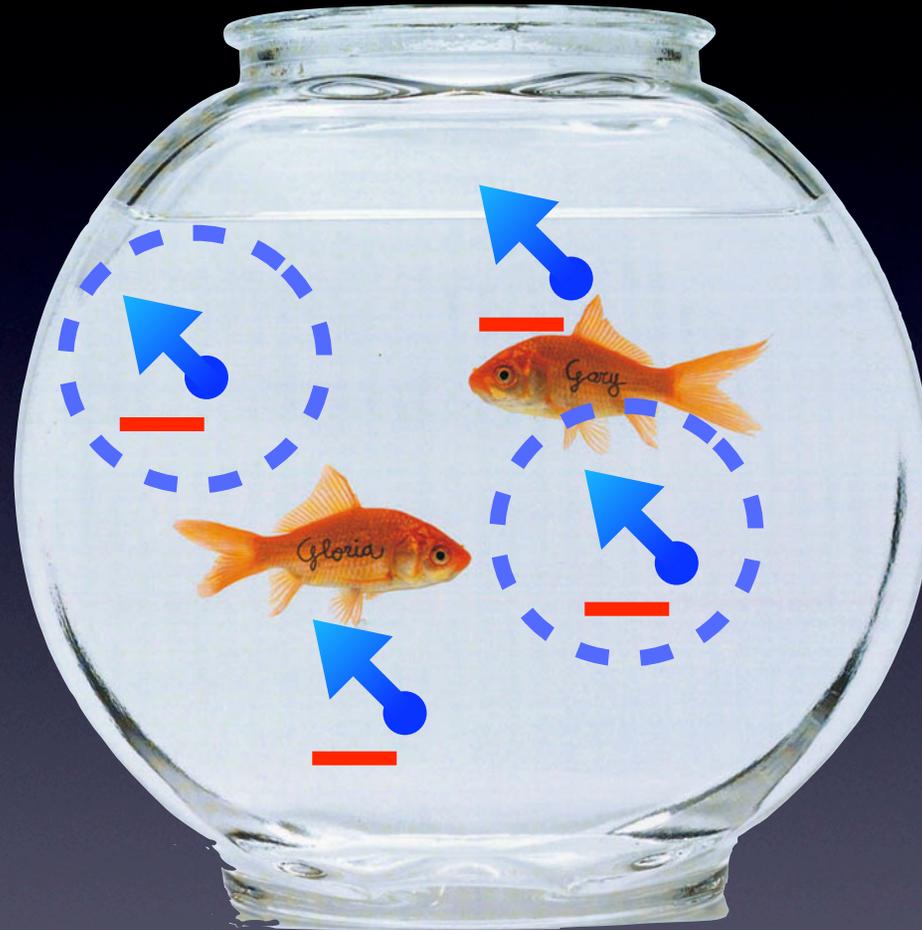
Diffusion



opposite
gradient

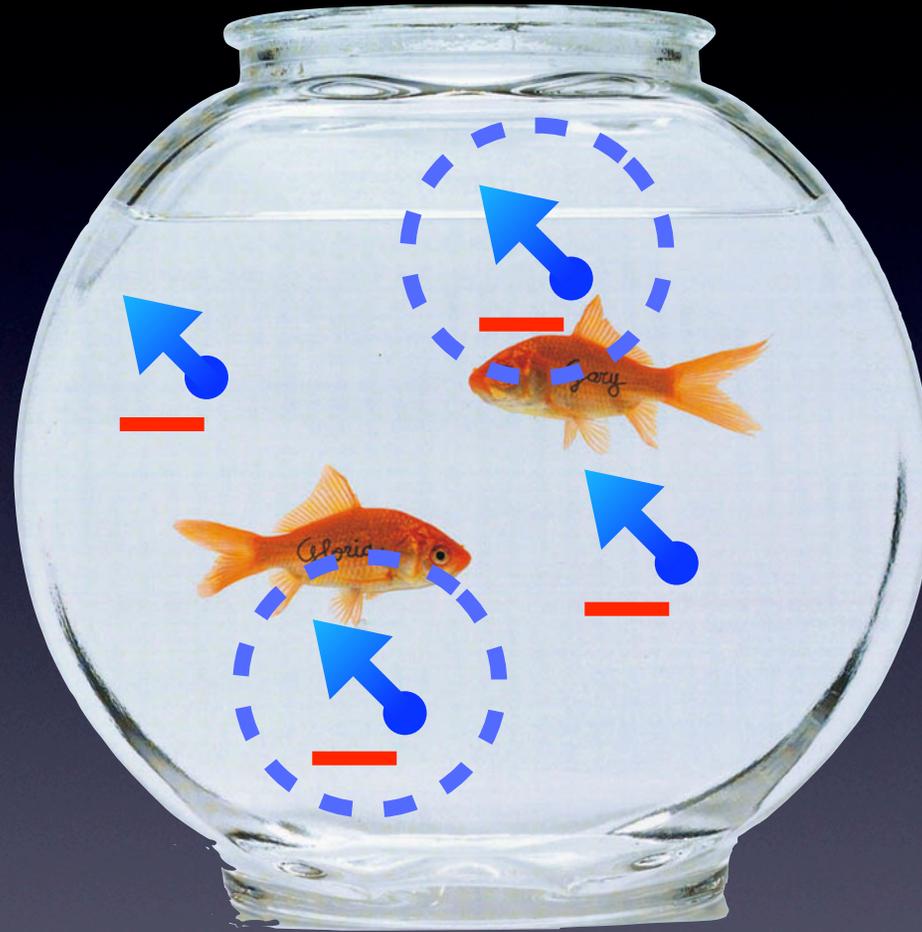
Diffusion

stationary =
re-focused



opposite
gradient

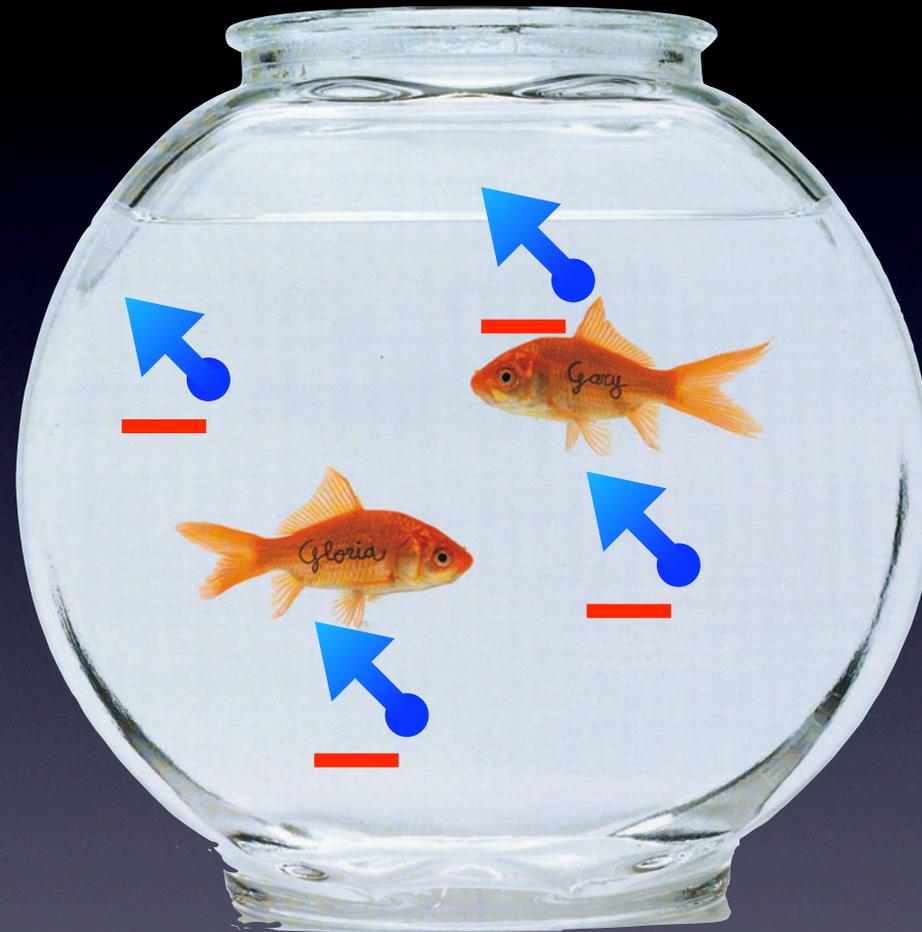
Diffusion



diffused =
re-focused

opposite
gradient

Diffusion



signal is unaffected by
diffusion perpendicular to the gradients

Diffusion imaging uses gradients to cancel out signal in water that moves in one direction.

Repeating the experiment, each time using gradient in a different direction, creates a map of how freely water diffuses in each voxel.

questions?

