

# OPTICAL COHERENCE TOMOGRAPHY

## INFERRING ARCHITECTONIC STRUCTURES AND CONNECTIVITY IN THE BRAIN

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## Great interest in architectonic structures

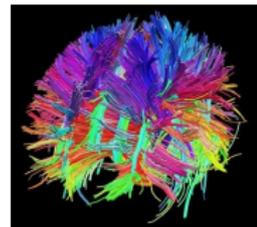
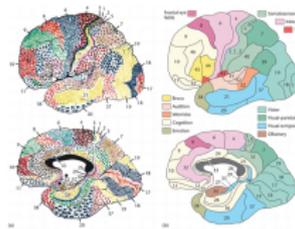
- diseases and disorders
- fMRI
- connectivity

⇒ Projects on *ex vivo* imaging

MRI (sequences, post processing, registration to *in vivo*)

- + whole brain
- + higher resolution
- + some architectonics structures revealed
- - brain dependant (aging, fixation, PMI...)
- - a lot of cortical areas can't be delimited

⇒ New direction: **OCT**



Histology (validation for MRI, guide)

- + whole brain
- + cellular resolution
- + gold standard for architectonic structures
- - labor intensive
- - distortions /deformations due to cutting, mounting and staining
- - different dyes for different interests (cells, myelinated fibers)

# NEW DIRECTION

- What is OCT ?
  - Optical: use of light
  - Coherence: use of low coherence interferometry
  - Tomography: 3D volume
- Why use OCT?
  - high resolution : up to 1  $\mu\text{m}$ 
    - ⇒ cells (neurons) : **cytoarchitecture**
    - ⇒ fibers : **myeloarchitecture & connectivity**
  - relies on intrinsic optical properties
    - ⇒ no staining
  - image the fixed blockface
    - ⇒ no or less deformation (compare to histology)

## 1 TISSUE OPTICS

- Basics
- Tissue Optical Window

## 2 OPTICAL COHERENCE TOMOGRAPHY

- Principle
- Spectral Domain OCT/OCM
- Image Processing

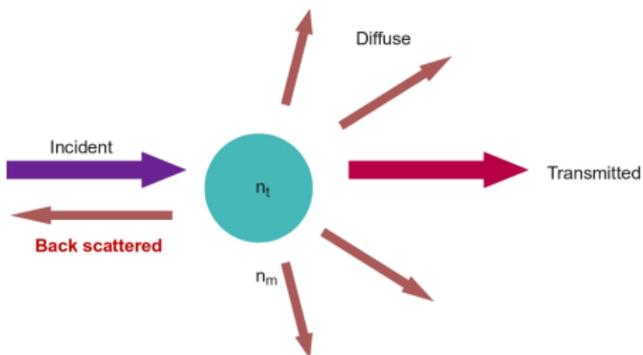
## 3 ARCHITECTONICS STRUCTURES

- Ex vivo MRI vs. OCT
- Cortical boundary
- Nissl Stain vs. OCT
- Assessment of deformations

## 4 CONNECTIVITY

- Principle and Process
- DTI vs. OCT
- Future work

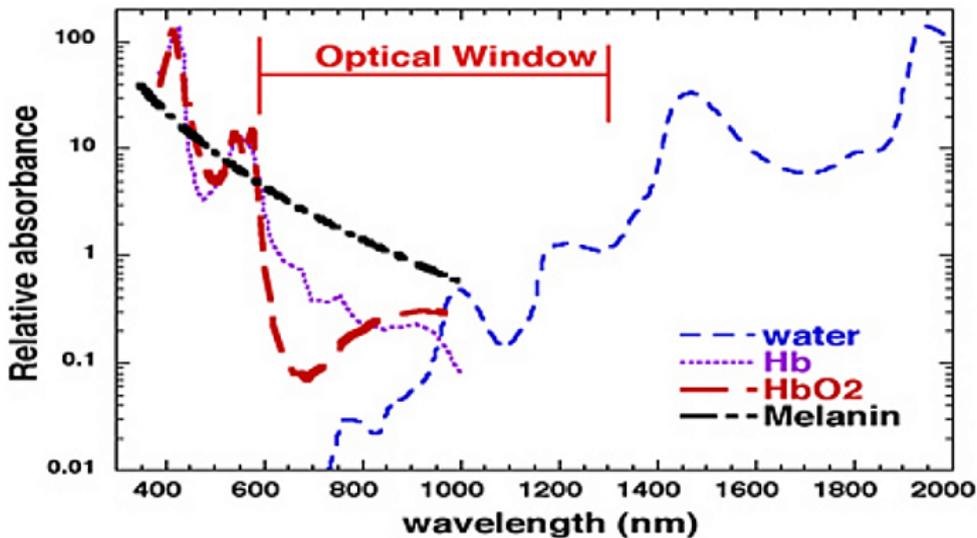
# TISSUE OPTICS : BASICS



- Cells (e.g. neurons)
- Myelinated fibers (the myelin sheath has a high refractive index)



# TISSUE OPTICAL WINDOW

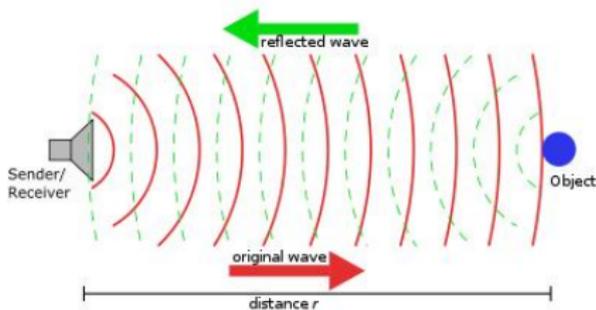


# OPTICAL COHERENCE TOMOGRAPHY

- ① Principle
- ② Spectral Domain OCT/OCM
- ③ Image Processing

# PRINCIPLE

- Introduced by Fujimoto <sup>1</sup>
- 3D technique with high resolution
- Analogue to UltraSound

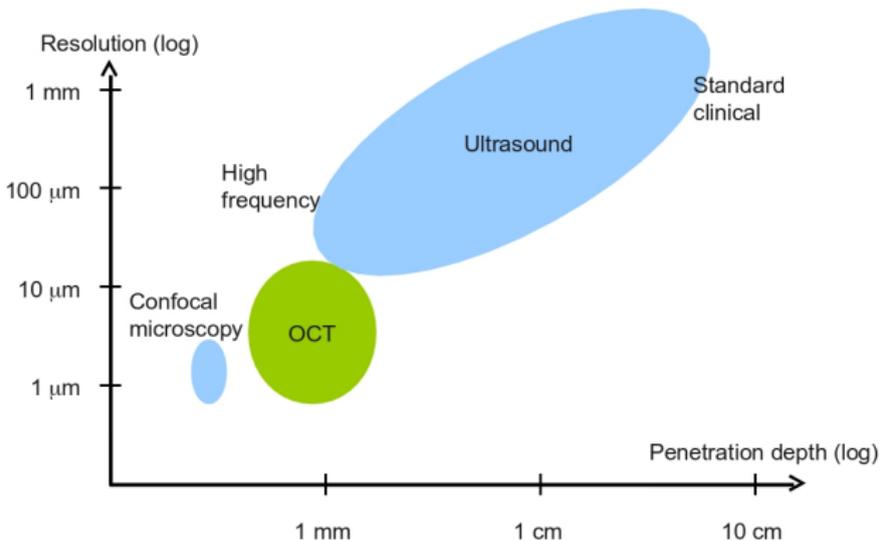


Speed of sound :  $1480 \text{ m}\cdot\text{s}^{-1}$  (in water)

Speed of light :  $3 \times 10^8 \text{ m}\cdot\text{s}^{-1}$

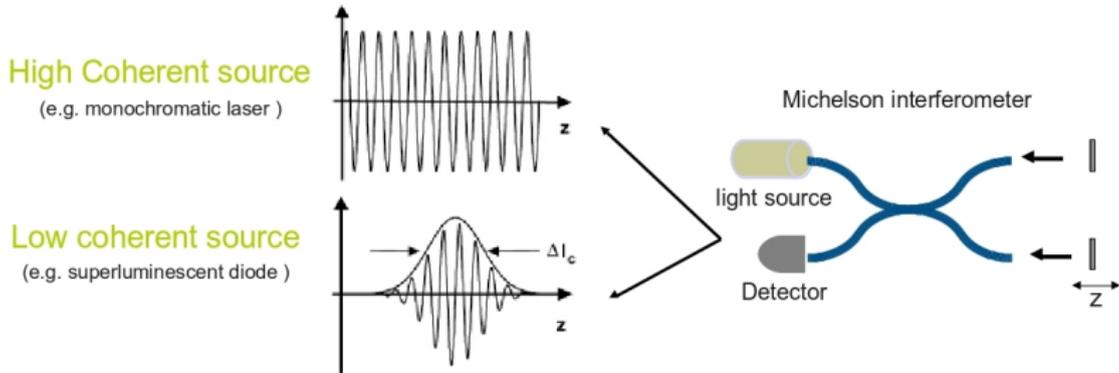
<sup>1</sup>David Huang, Eric A. Swanson, Charles P. Lin, Joel S. Schuman, William G. Stinson, Warren Chang, Michael R. Hee, Thomas Flotte, Kenton Gregory, Carmen A. Puliafito and James G. Fujimoto, "Optical Coherence Tomography," Science, Vol. 254, 1991.

# PRINCIPLE : RESOLUTION / PENETRATION

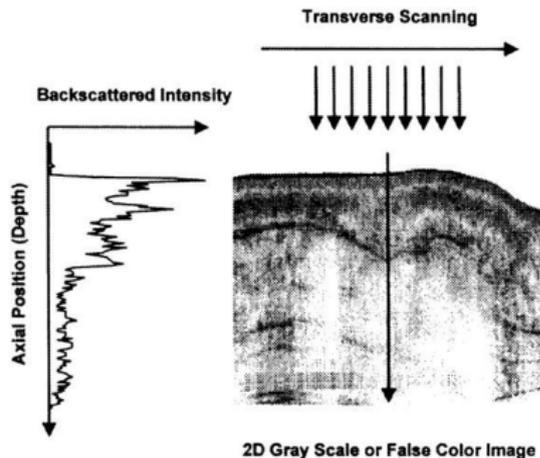
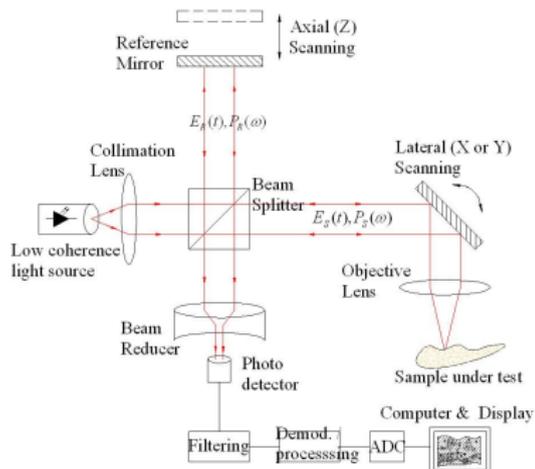


# PRINCIPLE : INTERFEROMETRY

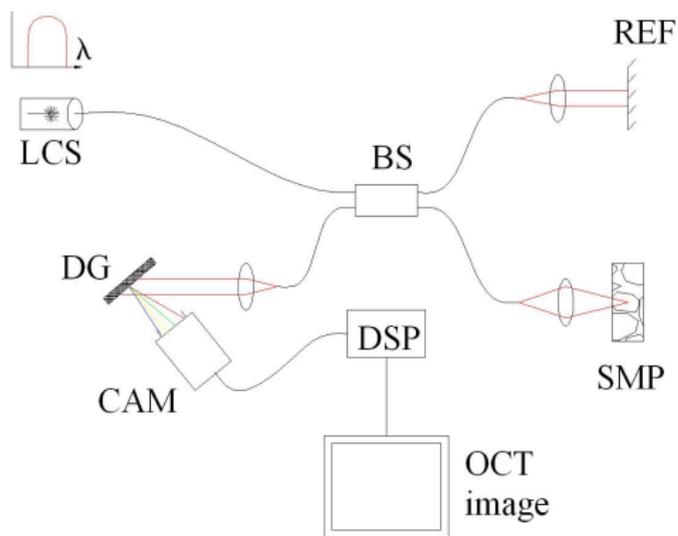
Light is too fast  $\Rightarrow$  Interference between the reflected light and a reference light



# PRINCIPLE : TIME DOMAIN OCT (TD-OCT)



# SPECTRAL DOMAIN OCT (SD-OCT)<sup>2</sup>



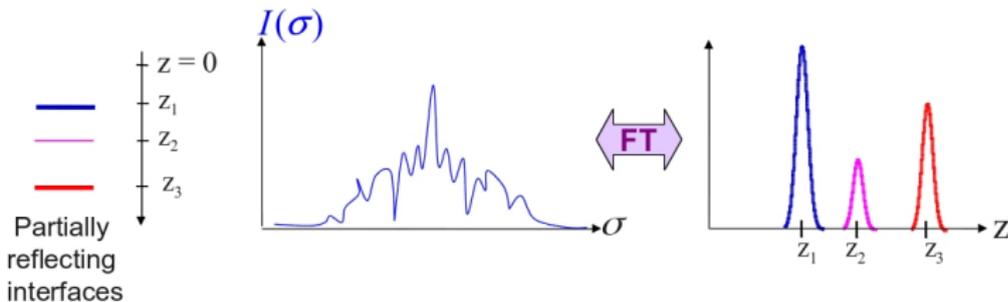
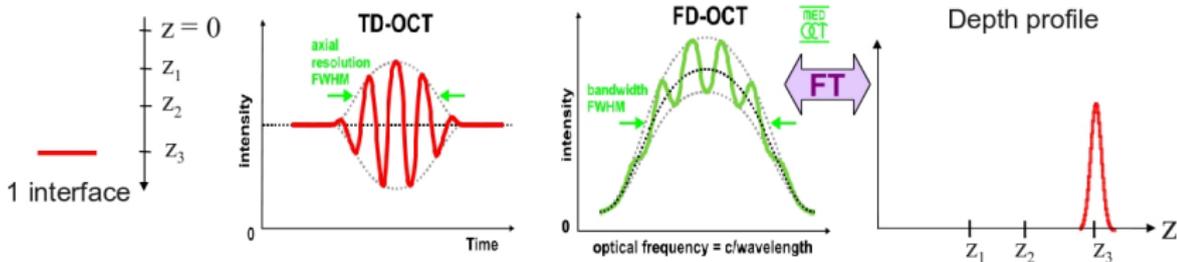
Optical Coherence Microscopy

Objective in the sample arm  
 ⇒ Better resolution

- No movement of the reference mirror
- Faster (1 spectra = 1depth profile)
- Reduced losses

<sup>2</sup>V. J. Srinivasan, et al., "Optical coherence microscopy for deep tissue imaging of the cerebral cortex with intrinsic contrast", Optics Express, 20(3), 2012

# SD-OCT vs TD-OCT

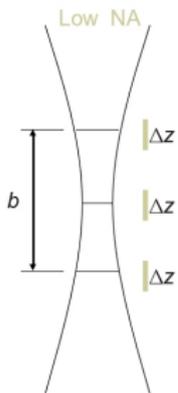
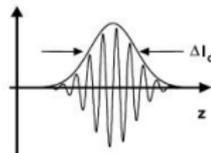


# EXAMPLE

# RESOLUTIONS AND DEPTH OF FOCUS

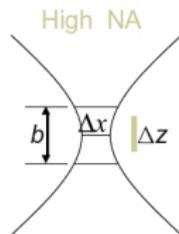
- Axial Resolution : depends on light source bandwidth  $\Delta\lambda$

$$l_c = \frac{2 \ln 2}{\pi} \frac{\lambda_0^2}{\Delta\lambda}$$



- Lateral Resolution : depends on the objective (Numerical Aperture)

$$\Delta x = \frac{2\lambda_0}{\pi NA}$$



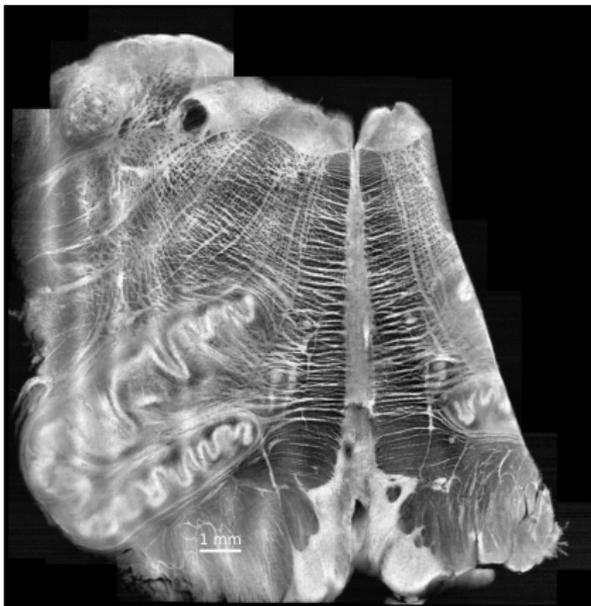
- Depth of focus : depends on the objective (Numerical Aperture)

$$b = \pi \frac{\Delta x^2}{2\lambda_0}$$

# EXAMPLE : MEDULLA (BRAIN STEM)

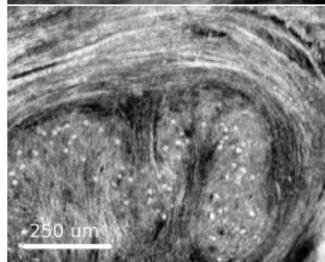
SuperLuminescent Diode (SLD)

- $\lambda_0 = 1310\text{nm}$
- $\Delta\lambda = 170\text{nm}$



**Obj. 10x, NA 0.3**

Axial res.  $3.5 \mu\text{m}$   
Lateral res.  $3 \mu\text{m}$   
Depth of focus  $20 \mu\text{m}$

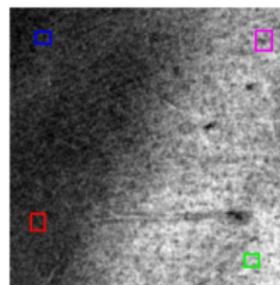
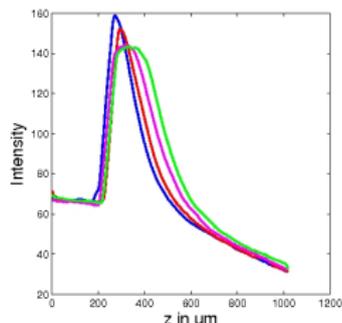
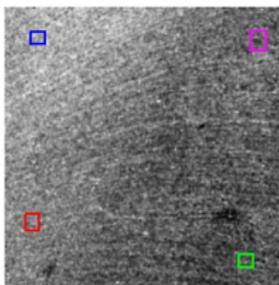


**Obj. 40x, NA 0.8**

Axial res.  $3.5 \mu\text{m}$   
Lateral res.  $1 \mu\text{m}$   
Depth of focus  $3 \mu\text{m}$

# IMAGE PROCESSING

- 1 acquired volume = 1.5 mm × 1.5 mm × 1.5 mm (10x obj.)
- Average Intensity Projection over 400  $\mu\text{m}$  below the surface
- Maximum Intensity Projection over 400  $\mu\text{m}$  below the surface
- XY translation stage
- Stitching: Fiji plug-in based on Fourier shift theorem <sup>3</sup>



<sup>3</sup>S. Preibisch, S. Saalfeld, P. Tomancak, "Globally optimal stitching of tiled 3D microscopic image acquisitions", Bioinformatics, 25(11), 2009

# IMAGE PROCESSING

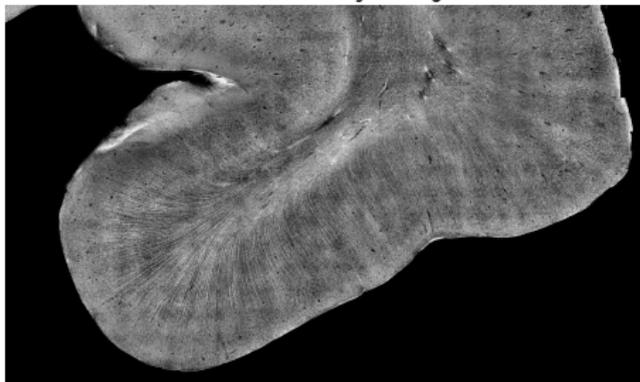
Isocortex, Brodmann areas 36 and 20

Average Intensity Projection



**Cytoarchitecture**

Maximum Intensity Projection



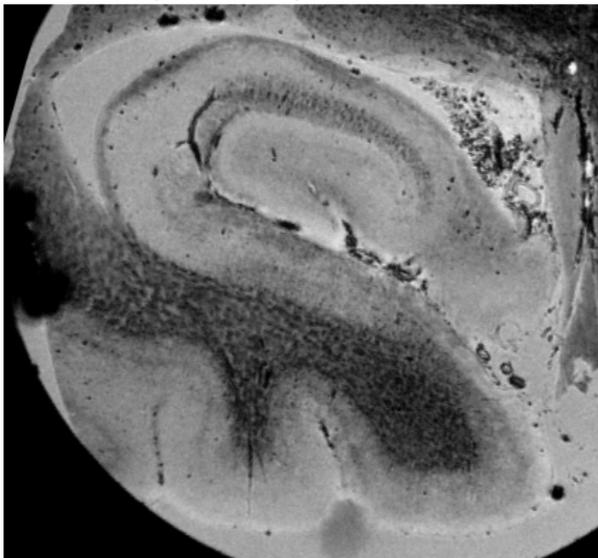
**Myeloarchitecture**

# ARCHITECTONICS STRUCTURES

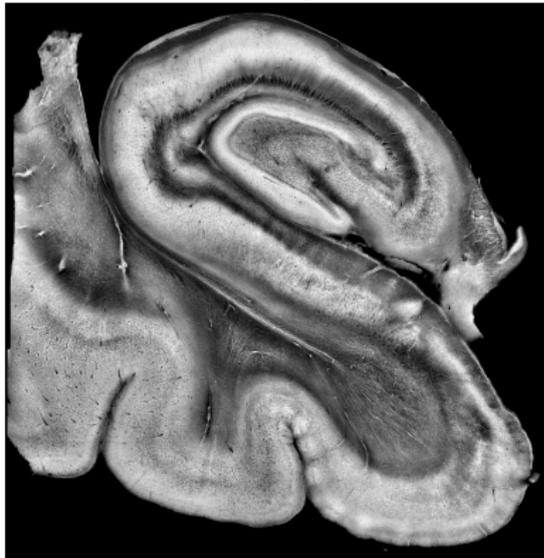
- 1 *ex vivo* MRI vs. OCT
- 2 Cortical boundary: EC / PC
- 3 Nissl stain vs. OCT: isocortex
- 4 Assessment of deformations

# *ex vivo* MRI vs. OCT: HIPPOCAMPUS

7T, FLASH,  $60 \mu\text{m}^3$ , TE=22ms,  
TR=55ms, FA=25°, 1 run



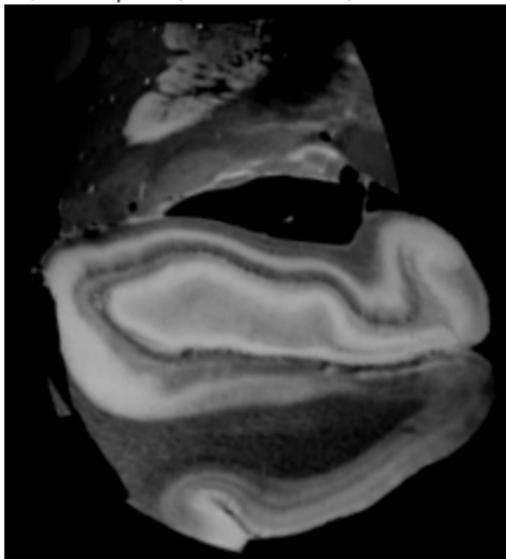
OCT  
lateral resolution:  $3 \mu\text{m}$



73 y.o., Male, PMI < 24hrs, length of fixation 4 months

# ENTORHINAL / PERIRHINAL CORTEX BOUNDARY

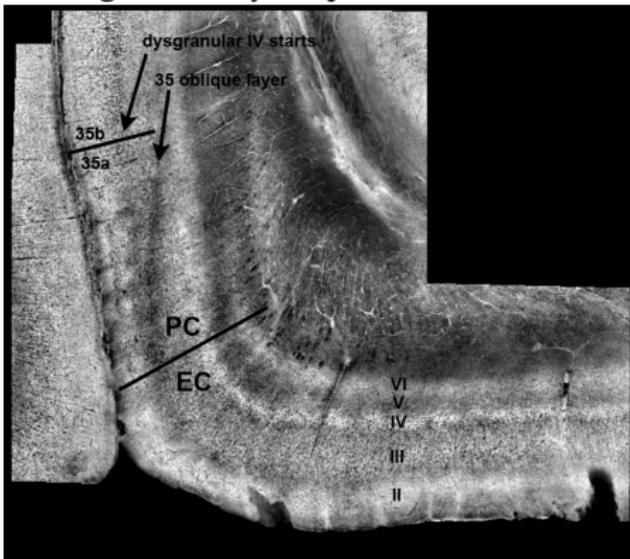
7T, FLASH,  $100 \mu\text{m}^3$ , TE=20ms, TR=40ms, FA=20°



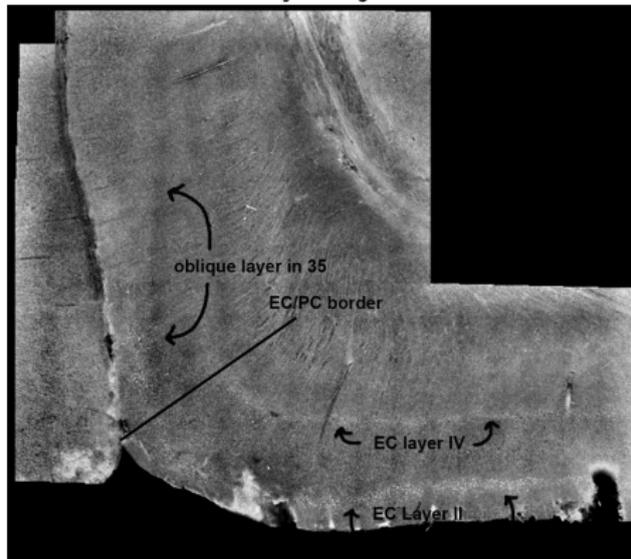
67 y.o., Male, PMI 12hrs

# ENTORHINAL / PERIRHINAL CORTEX BOUNDARY

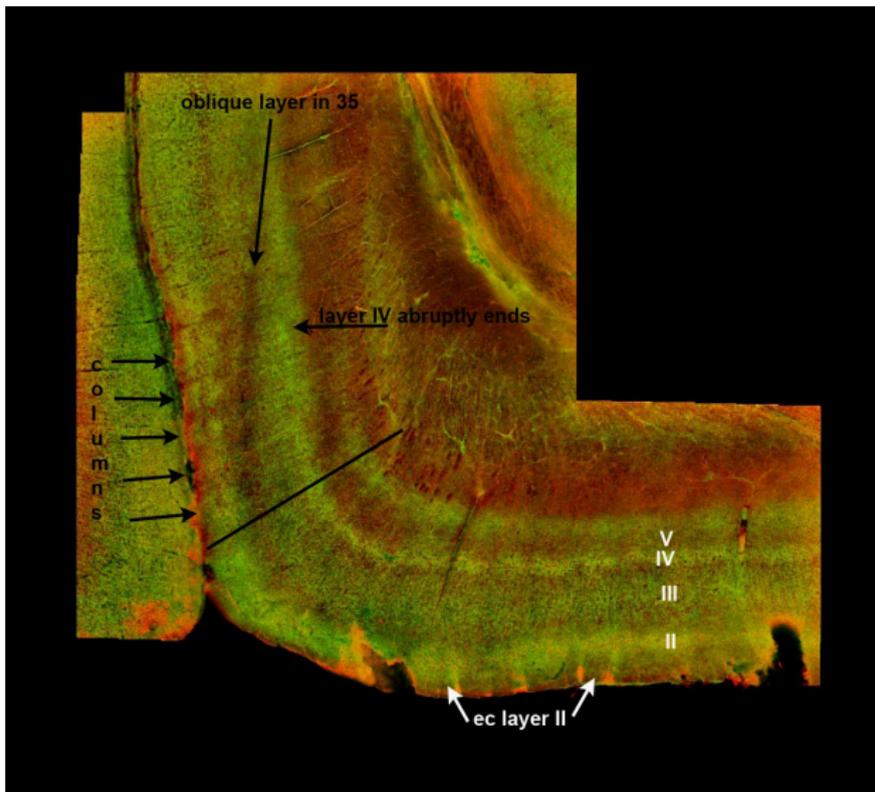
Average Intensity Projection



Maximum Intensity Projection



# ENTORRHINAL / PERIRRHINAL CORTEX BOUNDARY

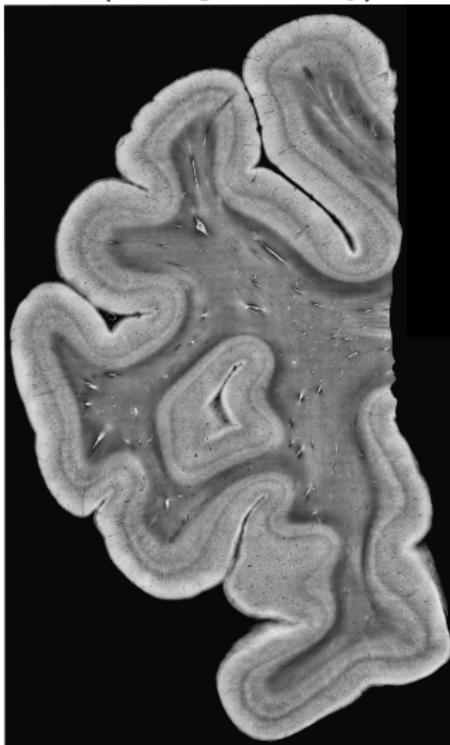


# NISSL STAIN *vs.* OCT: ISOCORTEX

Gold standard: Nissl stain

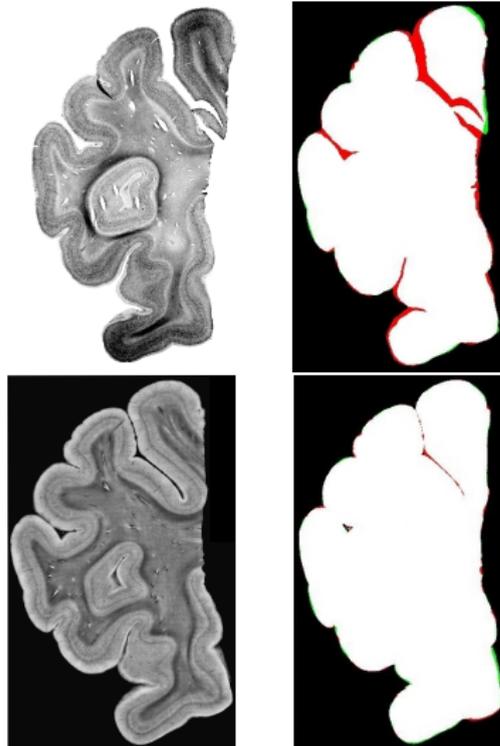


OCT (Average Intensity)



# DEFORMATIONS: REGISTRATION TO THE BLOCKFACE

Blockface



# CONNECTIVITY

## OCT-based Tractography

- 1 Principle and Process
- 2 Comparison with DTI

# PRINCIPLE AND PROCESS

- Maximum Intensity Projection
- Resolution for the Orientation Density Function (ODF) (*area*)
- Frequency Domain<sup>4</sup>
  - ① Hanning window
  - ② Padding (*pad*)
  - ③ Fourier Transform
  - ④ ODF reconstruction (*radius*)
  - ⑤ Preferential Direction(s) (*maxima of the ODF*)

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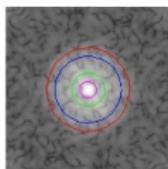
<sup>4</sup>C. J. Goergen, H. Radhakrishnan, D. E. Sosnovik, S. Sakadzi, and V. J. Srinivasan, "Optical coherence tractography using intrinsic contrast", *Optics Letters*, 37(18), 2012

# INFLUENCE OF RADIUS: SIMPLE CASE

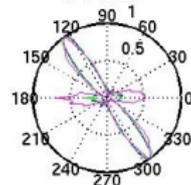
Area size 151  $\mu\text{m}$



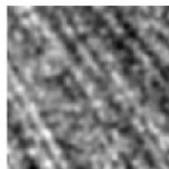
FT, pad 500 pix



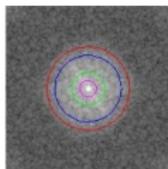
FT ODF



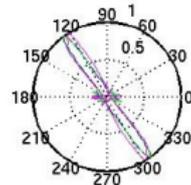
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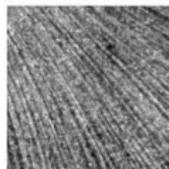
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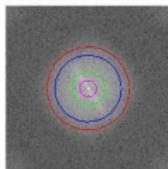
FT ODF



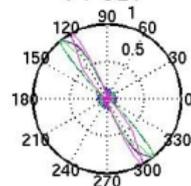
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FT, pad 500 pix

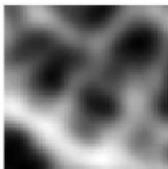


FT ODF

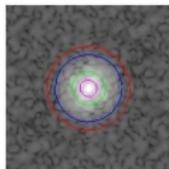


# MULTIPLE DIRECTIONS

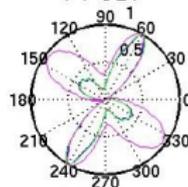
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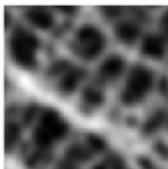
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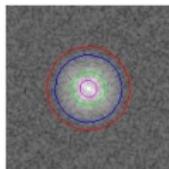
FT ODF



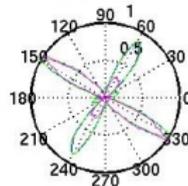
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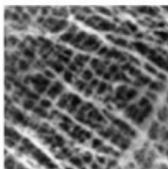
FT, pad 500 pix



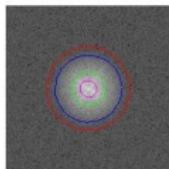
FT ODF



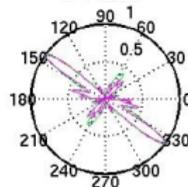
Area size 1001  $\mu\text{m}$



FT, pad 500 pix

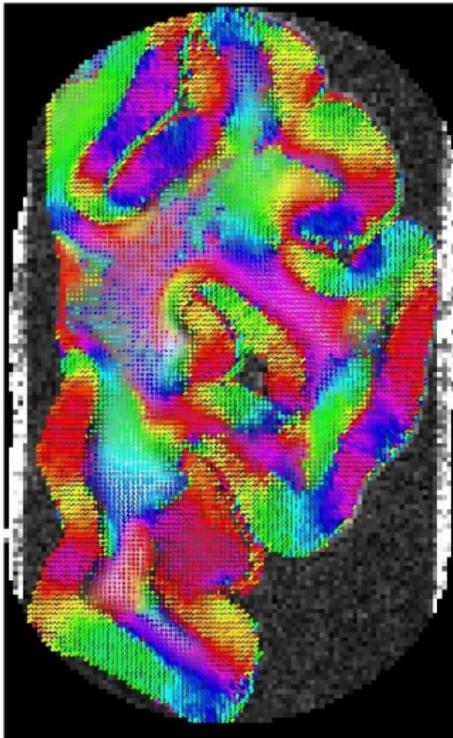


FT ODF

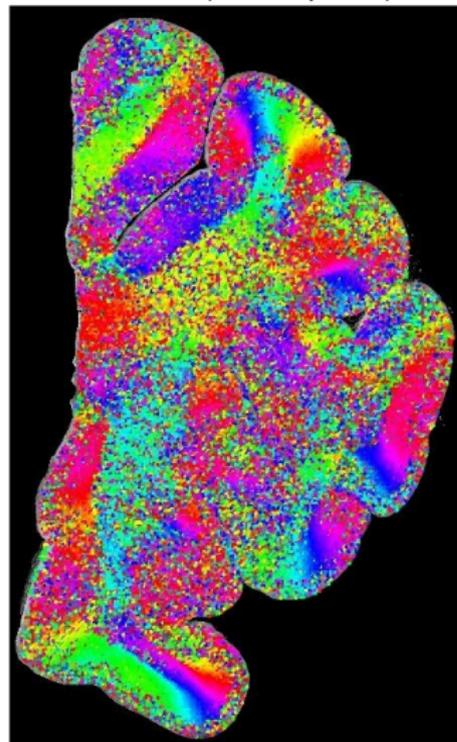


# DTI vs. OCT

DTI: 4.7T,  $300\mu\text{m}^3$ , 2 low-b img, 20 dir,  
 $b=2048$ ,  $TE=28\text{ms}$ ,  $TR=320\text{ms}$ ,  $FA=180^\circ$



OCT: lateral resolution =  $3\mu\text{m}$   
ODF :area  $300\mu\text{m}$ , step  $150\mu\text{m}$



# FUTURE WORK

- **3D reconstruction / 3D ODF**
  - **Vibrotome + XYZ Translation Stages**
    - Tim Ragan, Phil Knodle (Tissue Vision) <sup>5</sup>
    - Octopus
  - **Imaging a volume of human brain (several cm<sup>3</sup>)**
- **Registration with MRI**
- **Comparison with DTI and DSI**
- **Polarization-sensitive OCT** <sup>6</sup>

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<sup>5</sup>T. Ragan, J.D. Sylvan, K. Kim, et al, "High-resolution whole organ imaging using two-photon tissue cytometry," J. Biomed. Opt. 12(1), 2012.

<sup>6</sup>Wang, H., et al., "Reconstructing micrometer-scale fiber pathways in the brain: Multi-contrast optical coherence tomography based tractography", NeuroImage, 58(4), 2011.